



Image Analysis

Tim B. Dyrby

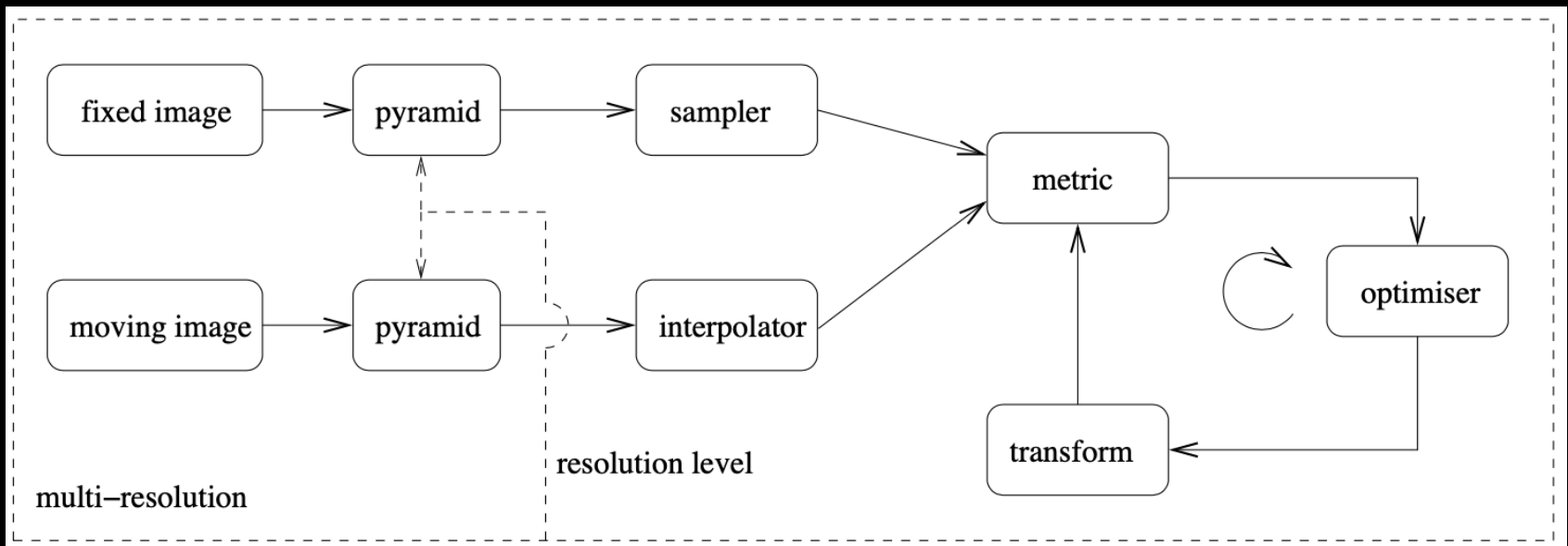
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Lecture 10 – Advanced image registration



Klein et al 2010. (IEEE Trans Med Img)

<https://elastix.lumc.nl>



What can you do after today?

- Describe difference between a pixel and voxel
- Choose a general image-to-image registration pipeline
- Apply 3D geometrical affine transformations
- Use the Homogeneous coordinate system to combine transformations
- Compute a suitable similarity metric given the image modalities to register
- Compute the normalized correlation coefficient (NNC) between two images
- Compute Entropy
- Describe the concept of iterative optimizers
- Compute steps in the gradient descent optimization steps
- Apply the pyramidal principle for multi-resolution strategies
- Select a relevant registration strategy: 2D to 3D, Within- and between objects and moving images



Go to www.menti.com and use the code 32 02 22 3

Associations to a mountain view



Mount Everest - Himalayas

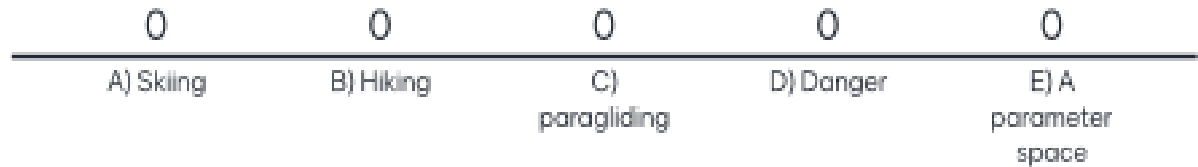


Image Registration pipeline

■ The input images

- Fixed image: Reference image
- Moving image: Template image

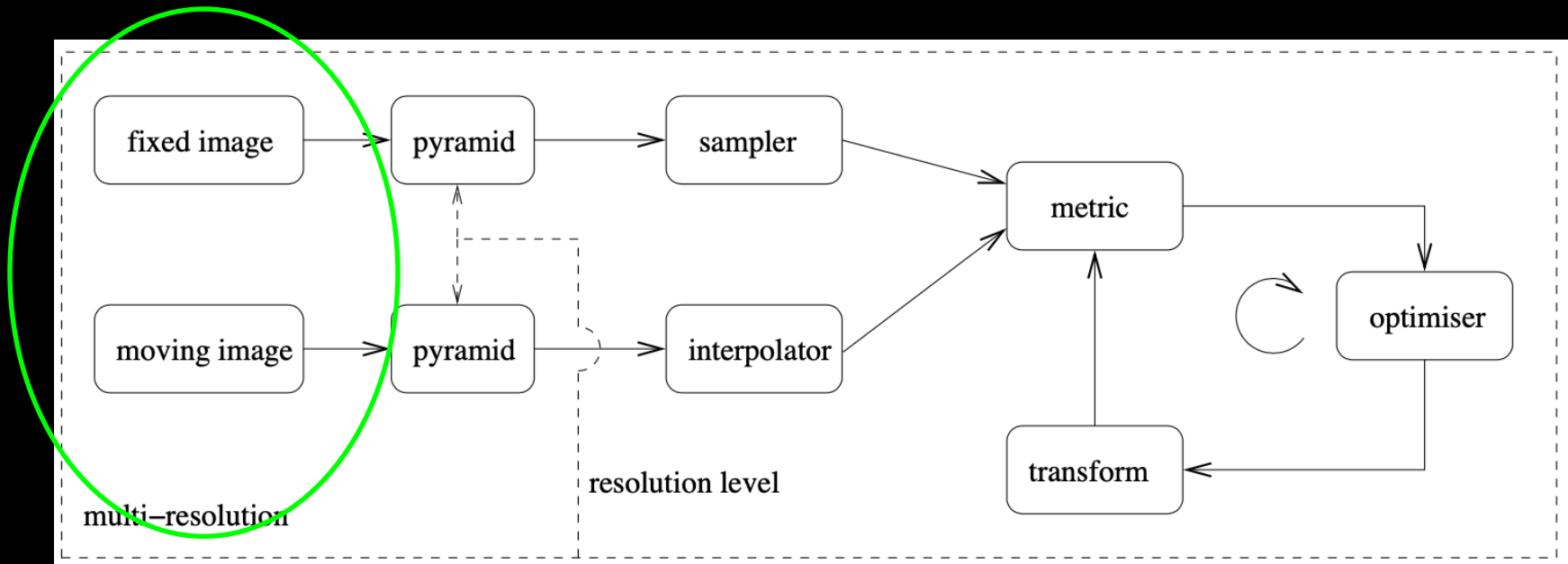
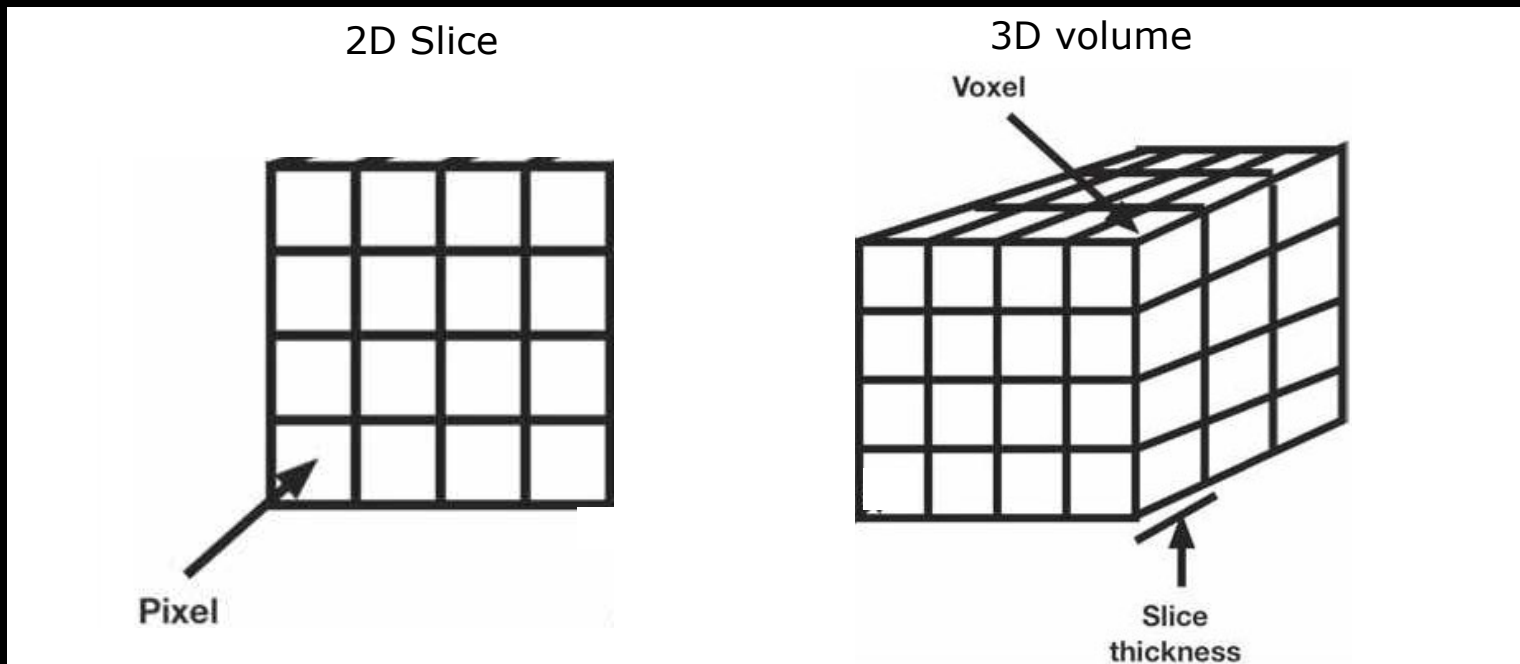


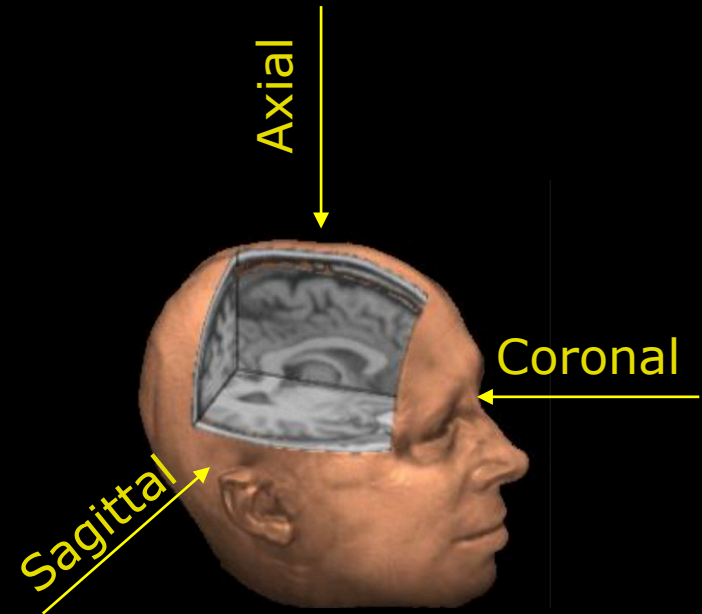
Image volumes

- Image slice: 2D ($N \times M$) matrix of pixels
- Image volumes: 3D ($N \times M \times P$) matrix of voxels
 - An element is a **volume pixel** i.e. voxel
- Pixel vs voxel intensity
 - Integrated information within an area or volume



3D image viewing

- Three orthogonal views
 - Fine structural details at slice level
 - Hard to get 3D surface insight
- Rendering of surfaces
 - Surface insight
 - Limited to clear surfaces

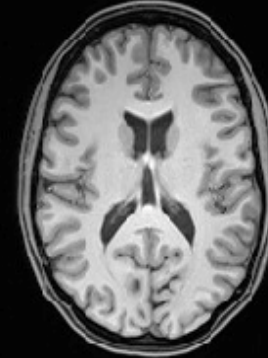
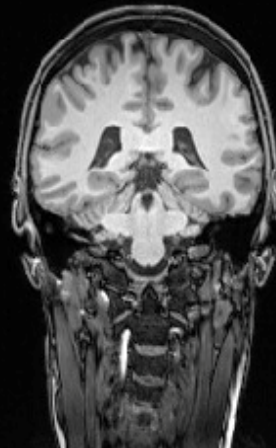


Slices three orthogonal views

Sagittal

Coronal

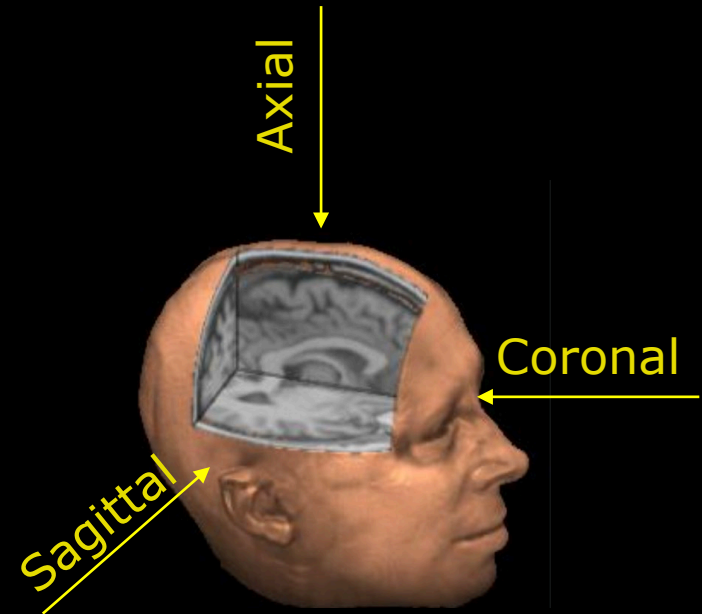
Axial





3D image viewing

- Three orthogonal views
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Slices three orthogonal views

Sagittal

Coronal

Axial



www.dreamstime.com/illustration/truck-top-view.html

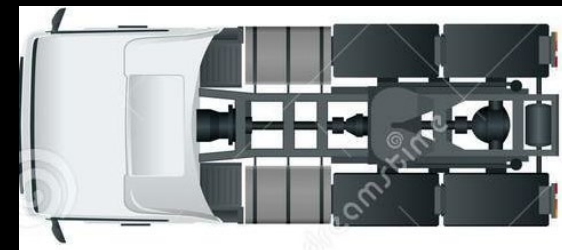
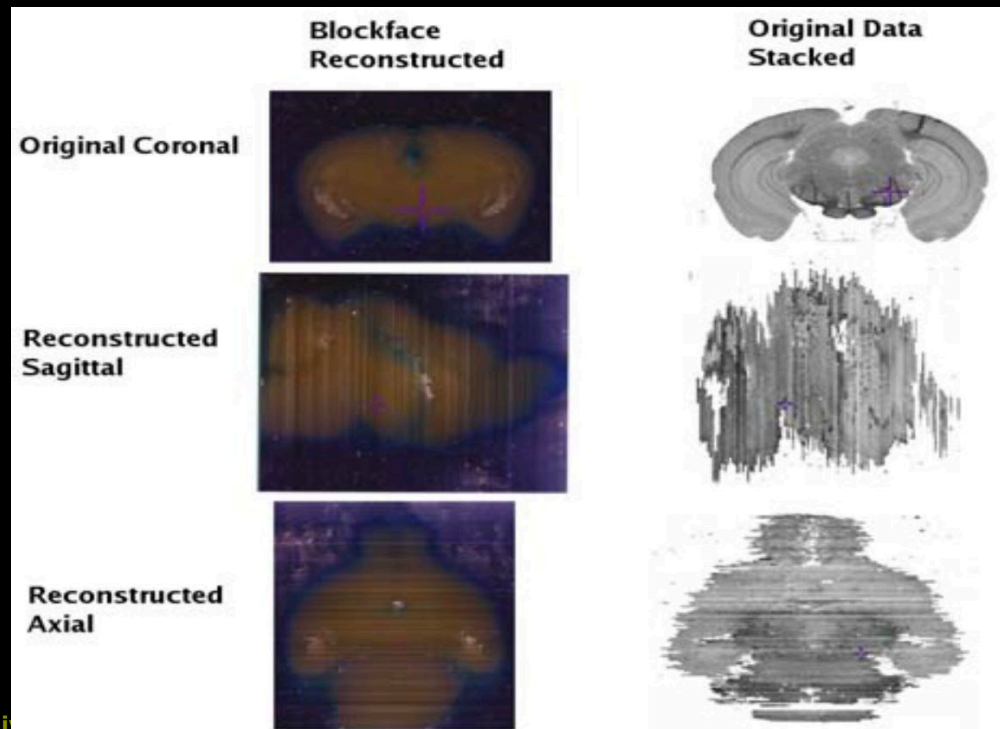




Image volumes

- Stacked slices: 2D to 3D
 - Object cut into slices, imaged and stacked
 - Still pixels – not voxel
- Registration challenges
 - Geometrical distortions between slices





Synchrotron x-ray imaging Tissue sample 1mm 75 nm isotropic resolution voxels

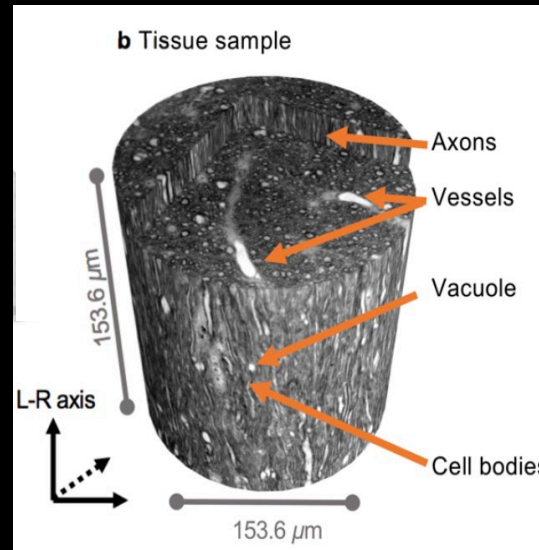
Image volumes

- Intact sample
 - No sample cutting
- Registration challenges:
 - Stacking 3D volumes

MRI

Whole brain

1 mm isotropic resolution voxels



Andersson et al, 2020 (PNAS)

Stacked 3D volumes

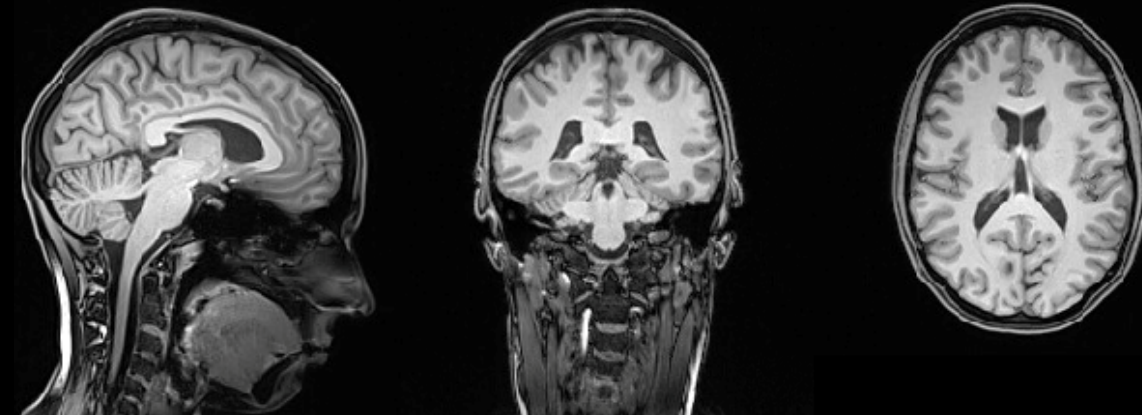
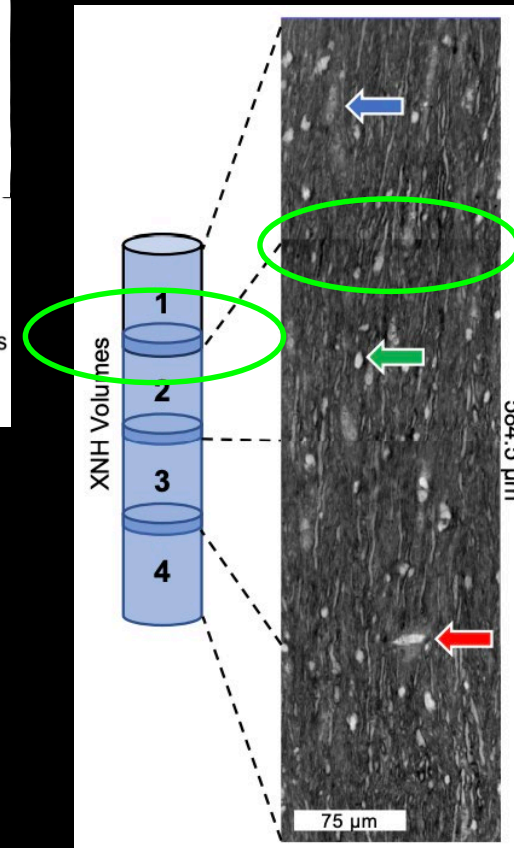
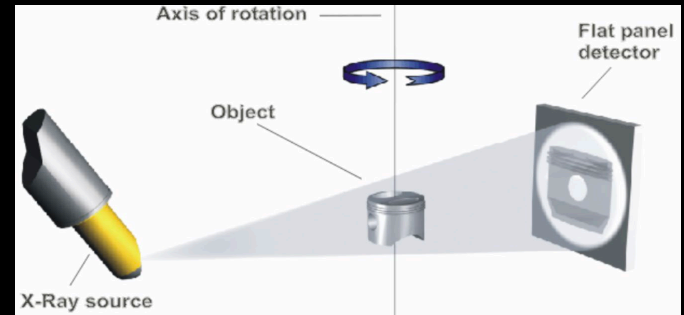


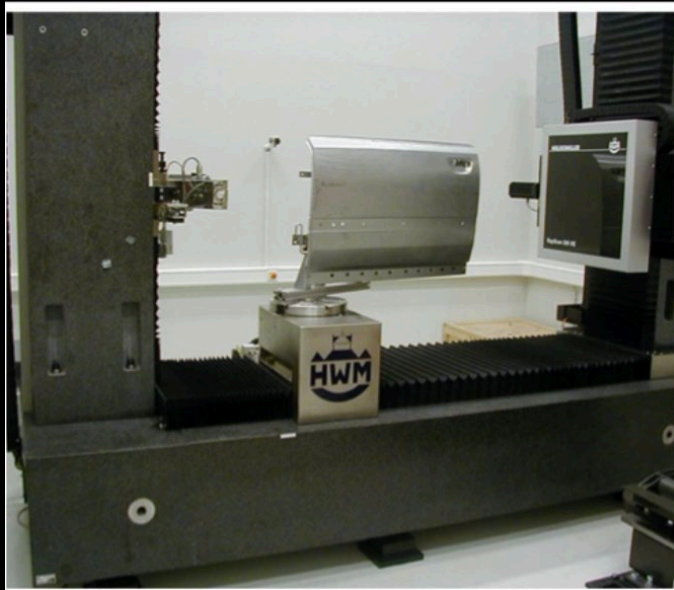
Image volumes

- Intact sample
 - No sample cutting
- Registration challenges:
 - Multi image resolution: Fit Region-of-interest image to whole object image

Rotating sample in x-ray tomography

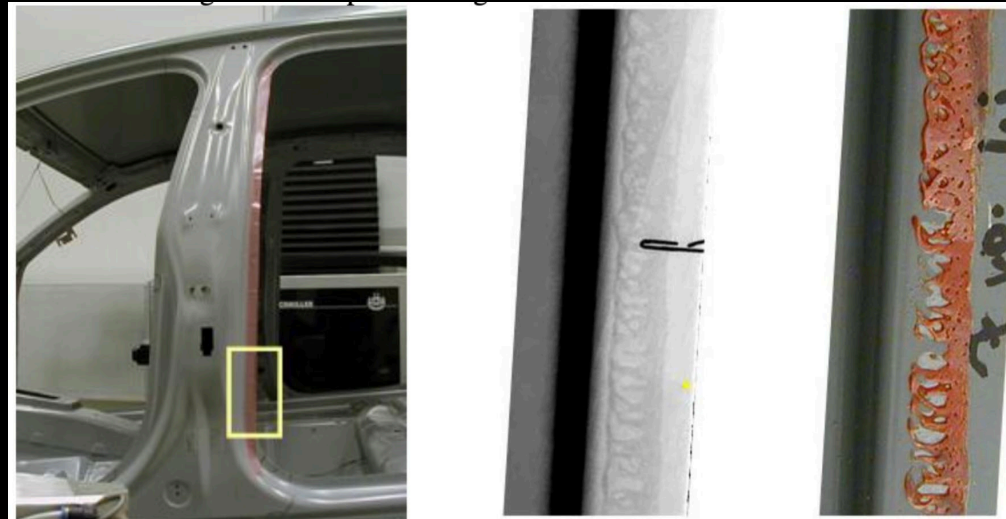


CT scanning



Car door AUDI A8, size: 1150 mm

Region of interest (ROI)	CT of ROI (non-destructive)	Microscope (destructive)
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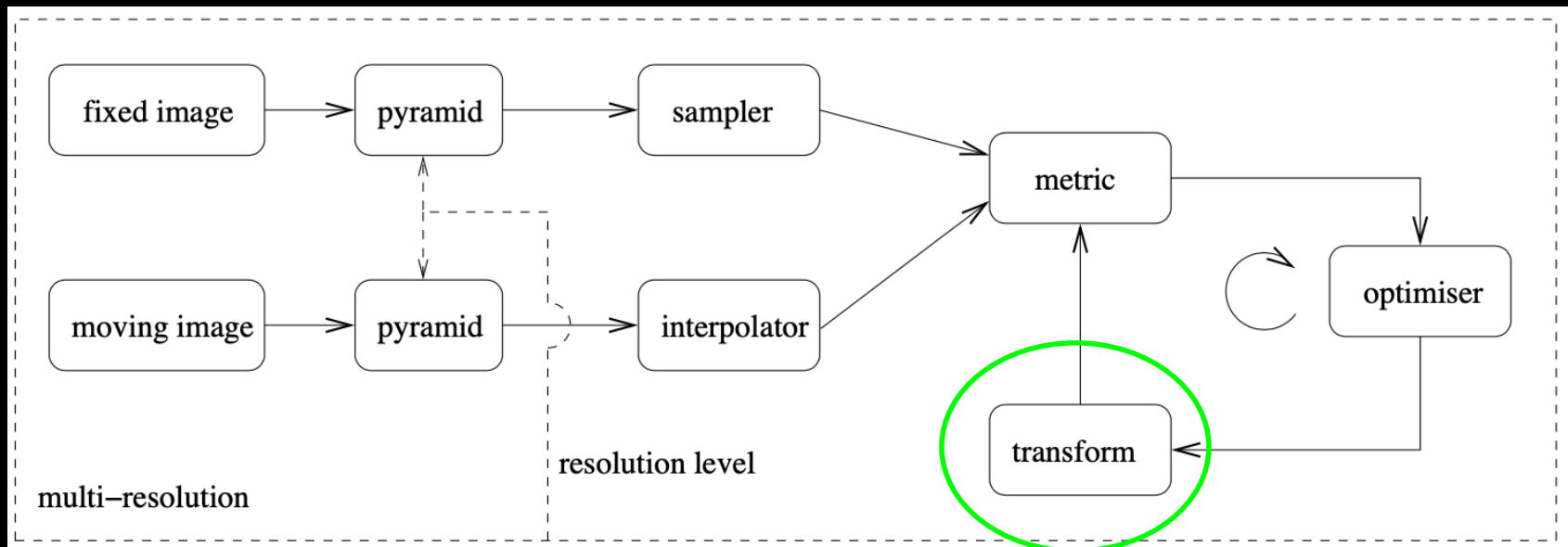


The inspection of a glued joint of a car body

Simon et al, 2006 (ECNDT)

Image Registration pipeline

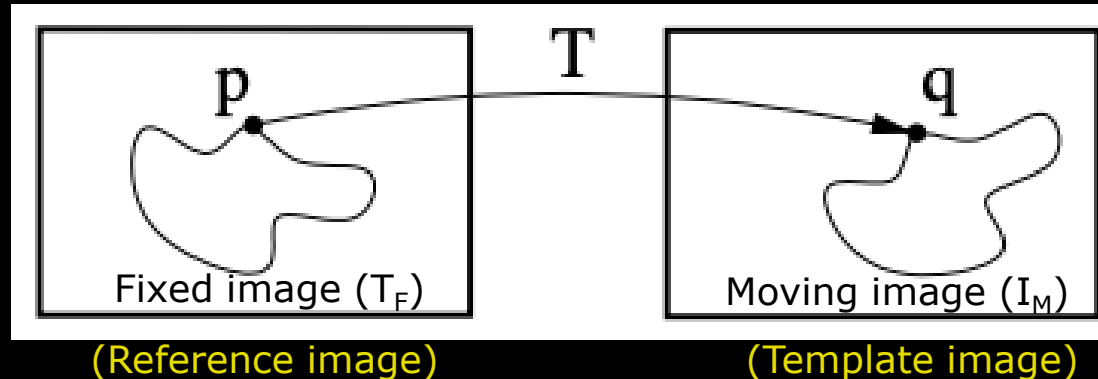
■ Geometrical transformations





Geometric transformations

- Translation
- Rotation
- Scaling
- Shearing



$$\hat{T} = \arg \min_T C(T; I_F, I_M)$$



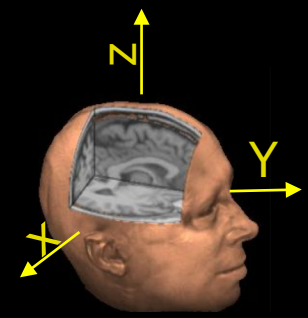
Translation 2D vs 3D

■ The image is shifted

- 2D: Inspect one slice plan
- 3D: Inspect three slice plans

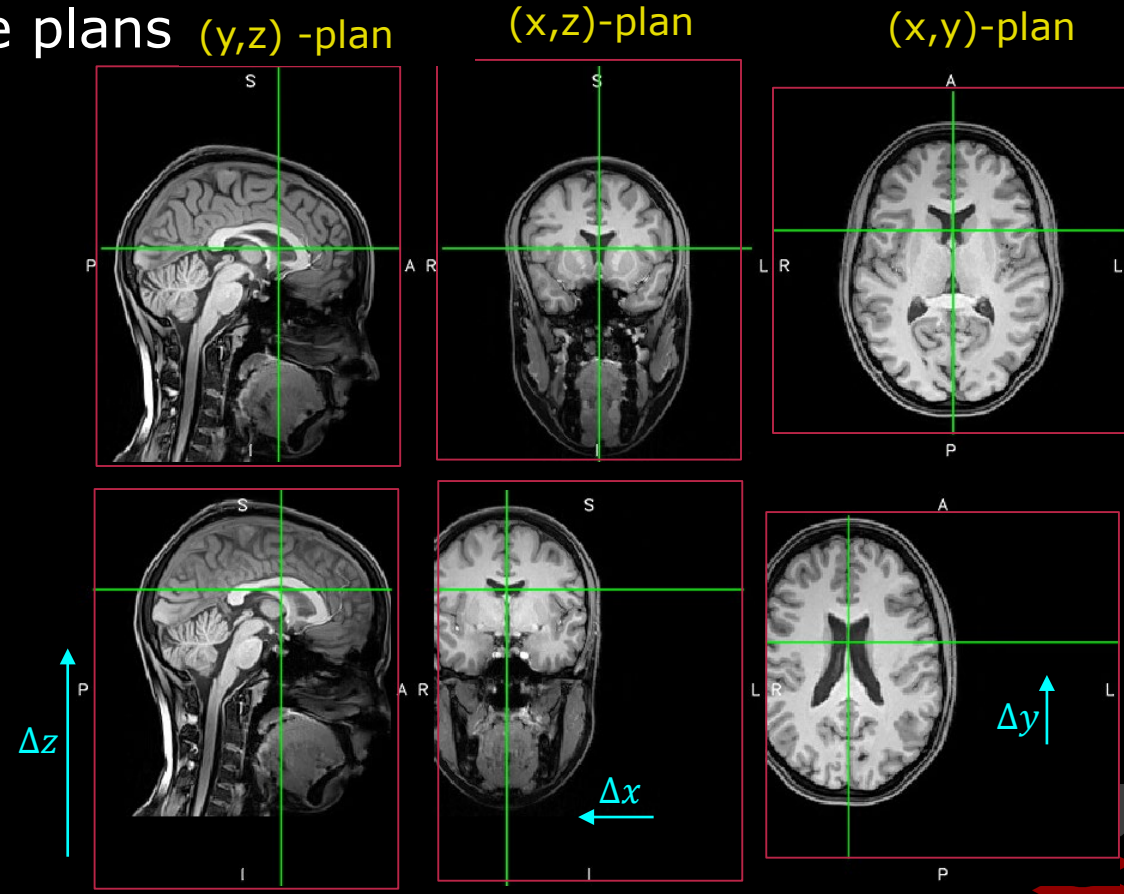
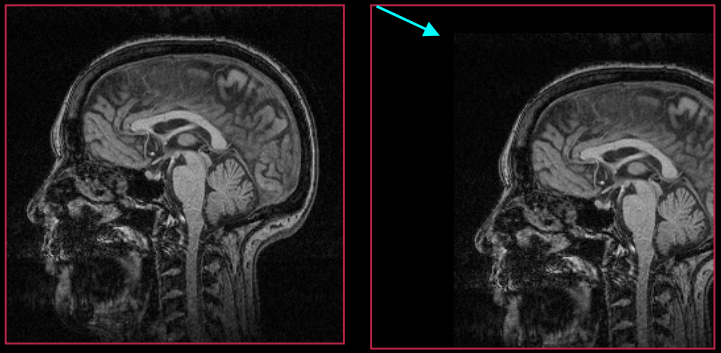
3D: (x,y,z)-plans

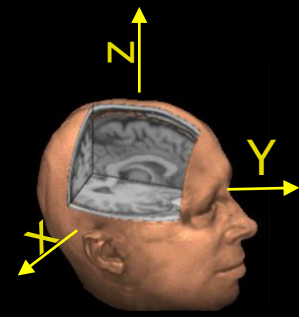
$$\begin{bmatrix} \Delta x \\ \Delta y \\ \Delta z \end{bmatrix} = - \begin{bmatrix} 60 \\ 20 \\ 15 \end{bmatrix}$$



2D: (x,y)-plan

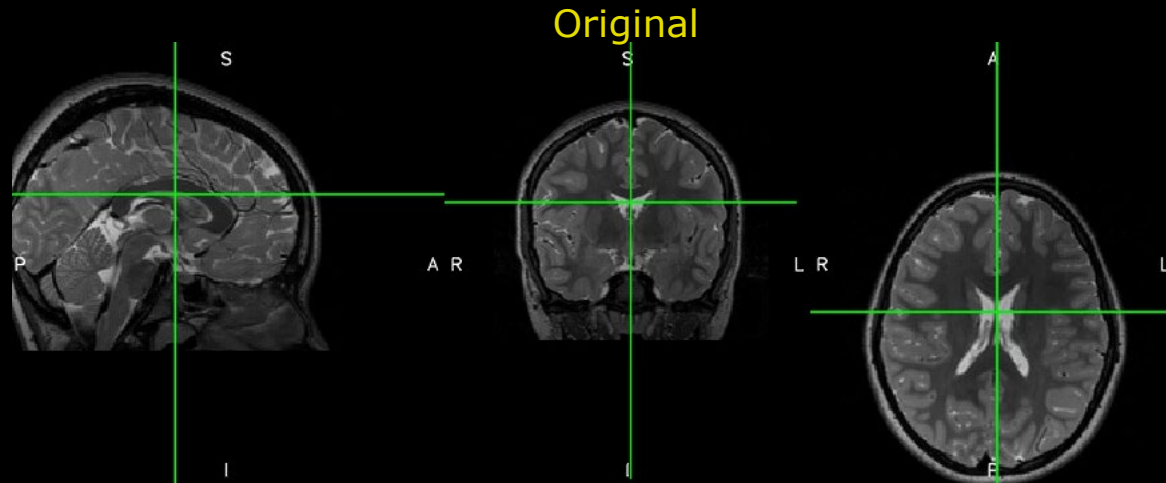
$$\begin{bmatrix} \Delta x \\ \Delta y \end{bmatrix} = \begin{bmatrix} 60 \\ 20 \end{bmatrix}$$



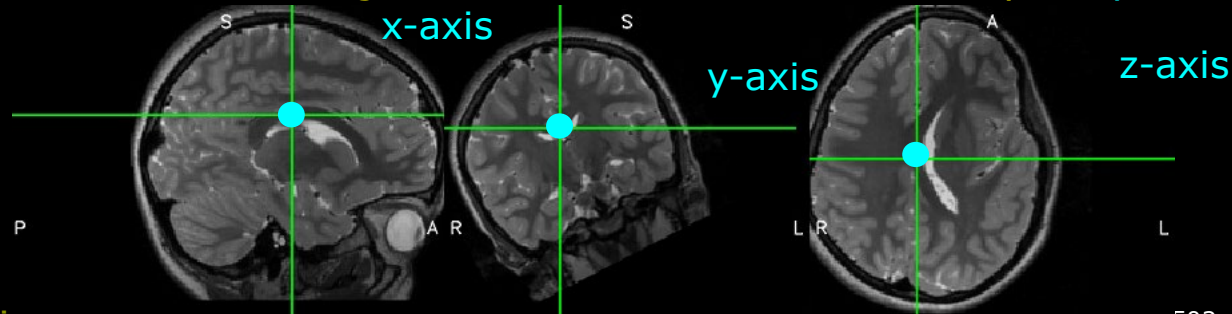


Rotation 3D

- The image is rotated around an origin (e.g. the centre-of-mass)
- Rotate the object around three axis hence three angles.
 - Inspect all three views to identify a rotation

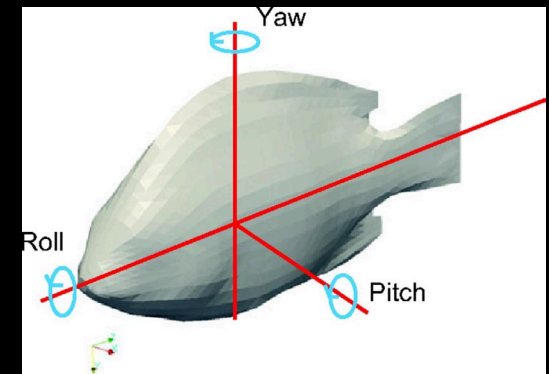
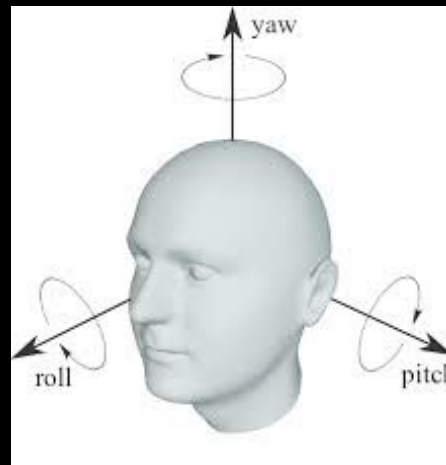
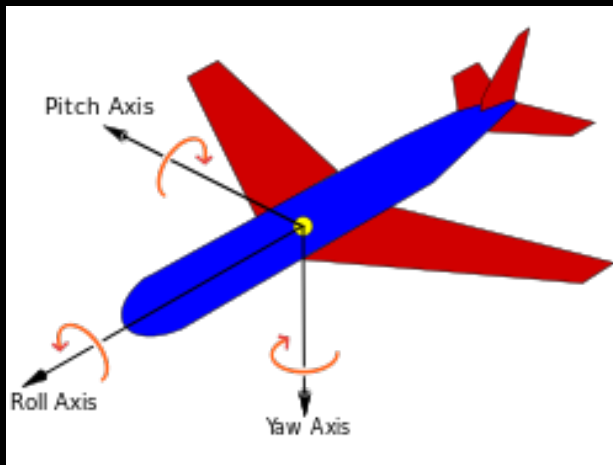


Rotated: 27 degree counter-clockwise around only the y-axis



3D Rotation coordinate system

- Three element rotations round the axes of the coordinate system
- Pitch, Yaw and Roll
 - Defined differently for different systems (typ. related to the forward direction)

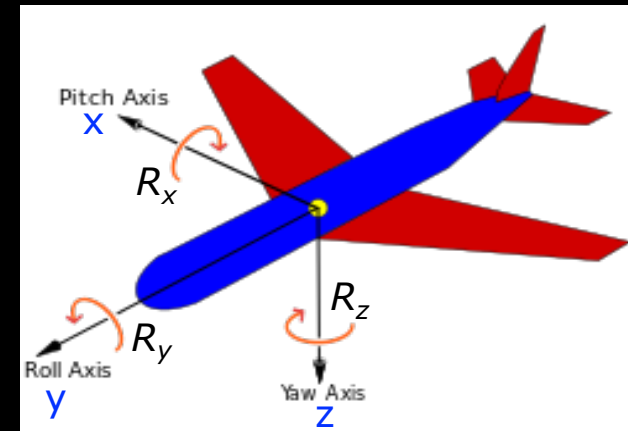


The principal axes of an aircraft according to the air norm DIN 9300

3D Rotation coordinate system

- Three composed element rotations
 - Angles: α, β, γ
- The order matters
 - Several conventions exist
- Remember: Know your origin!

Axis-Angle representation



$$\mathbf{R}_X = \begin{bmatrix} 1 & 0 & 0 \\ 0 & \cos \alpha & -\sin \alpha \\ 0 & \sin \alpha & \cos \alpha \end{bmatrix} \quad \mathbf{R}_Y = \begin{bmatrix} \cos \beta & 0 & \sin \beta \\ 0 & 1 & 0 \\ -\sin \beta & 0 & \cos \beta \end{bmatrix} \quad \mathbf{R}_Z = \begin{bmatrix} \cos \gamma & -\sin \gamma & 0 \\ \sin \gamma & \cos \gamma & 0 \\ 0 & 0 & 1 \end{bmatrix}$$

Pitch

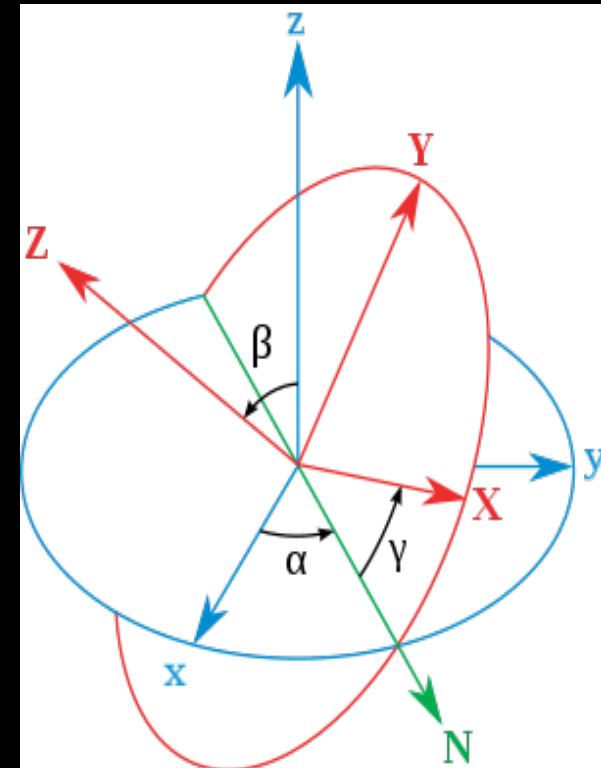
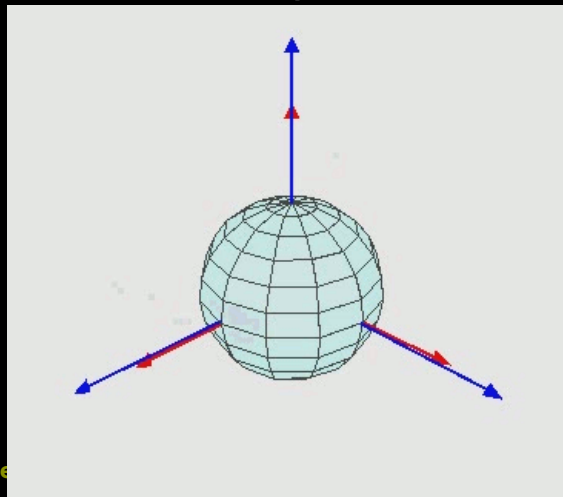
Roll

Yaw



3D Rotation coordinate system

- The Euler angel convention:
 - α : Around the **z-axis**. Defines the **line of nodes (N)**
 - β : Around the **X-axis** defined by **N**
 - γ : Around the **Z-axis** from **N**
- The order of coordinate system rotations:
 - Rotation order around the:
 - **z-axis**: Initial: Original frame (x,y,z): α
 - **X-axis**: First coordinate system rotation (X,Y,Z): β
 - **Z-axis**: Second coordinate system rotation (X,Y,Z): γ



wikipedia.org/wiki/Euler_angles



Quiz 1: Affine 3D transformation

How many parameters?

A) 6

B) 5

C) 16

D) 12

E) 3

SOLUTION:

Translation: $p=3$

Rotation: $p=3$

Scaling: $p=3$

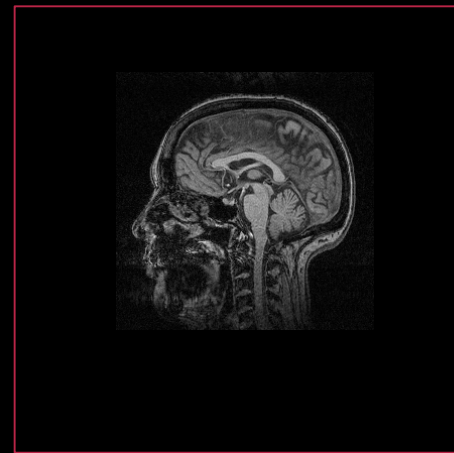
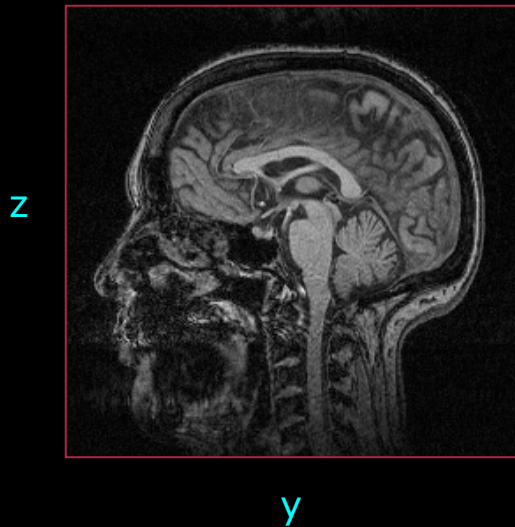
Shearing: $p=3$



Scaling in 3D

- The size of the image is changed
- Three parameters:
 - X-scale factor, S_x
 - Y-scale factor, S_y
 - Z-scale factor, S_z
- Isotropic scaling:

$$A = \begin{bmatrix} S_x & 0 & 0 \\ 0 & S_y & 0 \\ 0 & 0 & S_z \end{bmatrix}$$



$$A = \begin{bmatrix} 0.5 & 0 & 0 \\ 0 & 0.5 & 0 \\ 0 & 0 & 0.5 \end{bmatrix}$$

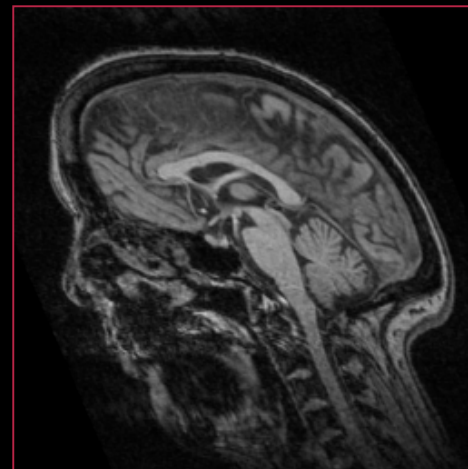
Shearing in 3D

- Pixel shifted horizontally or/and vertically
- Three parameters

$$A = \begin{bmatrix} 1 & S_{yx} & S_{zx} \\ S_{xy} & 1 & S_{yz} \\ S_{xz} & S_{yz} & 1 \end{bmatrix}$$



Shearing (z,y)-plan





Combining transformations

Translation:

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = \begin{bmatrix} \Delta x \\ \Delta y \\ \Delta z \end{bmatrix} + \begin{bmatrix} x \\ y \\ z \end{bmatrix}$$

Rotations,
Scaling,
Shear:

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = A \begin{bmatrix} x \\ y \\ z \end{bmatrix}$$

- Translation is a *summation* i.e. $P' = A + P$
- Rotation, Scale, Shear are *multiplications* i.e. $P' = A * P$

- Combine transformations multiplications:

$$A = A_T * A_R * A_{shear} * A_S$$

- Not possible with A_T



Homogeneous coordinates

Cartesian coordinates:

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = A \begin{bmatrix} x \\ y \\ z \end{bmatrix}$$

Homogeneous coordinates:

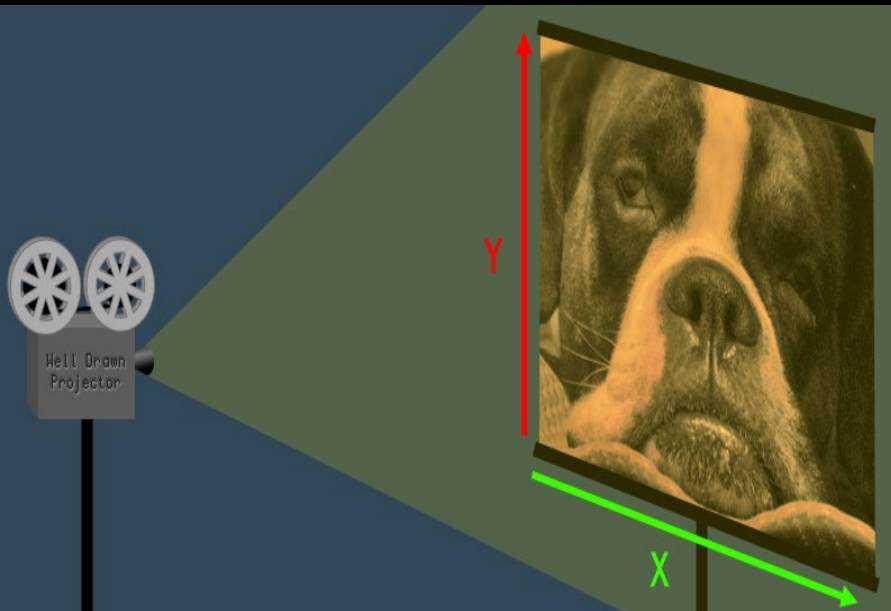
$$\begin{bmatrix} x' \\ y' \\ z' \\ w \end{bmatrix} = A \begin{bmatrix} x \\ y \\ z \\ w \end{bmatrix}$$

- Projective geometry
 - Used in computer vision
- Adds an extra dimension to vector, W :

$$[x, y, z, w]$$

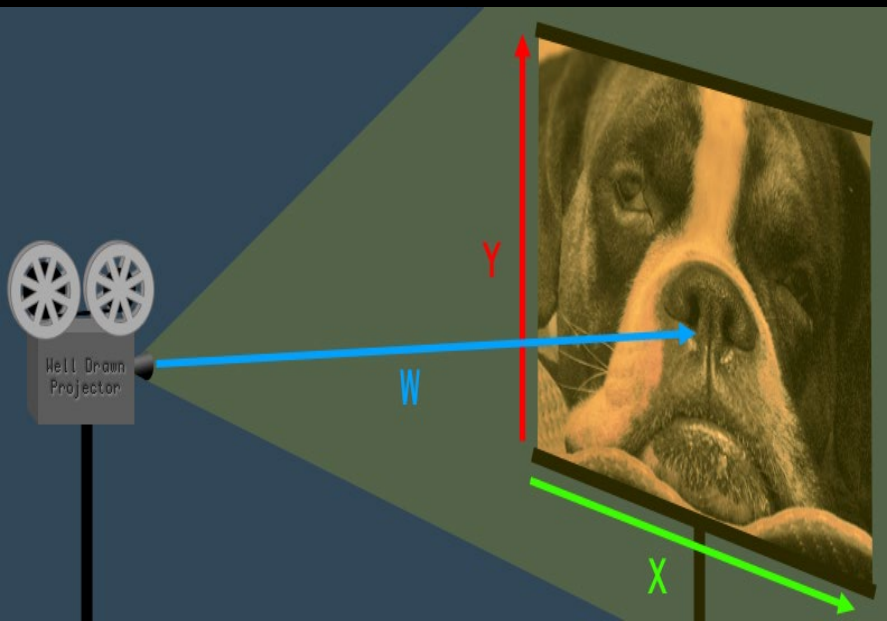
- How does it work?

Homogeneous coordinates



- Euclidean geometry: (x,y)
 - A 2D image
 - Cartesian coordinates

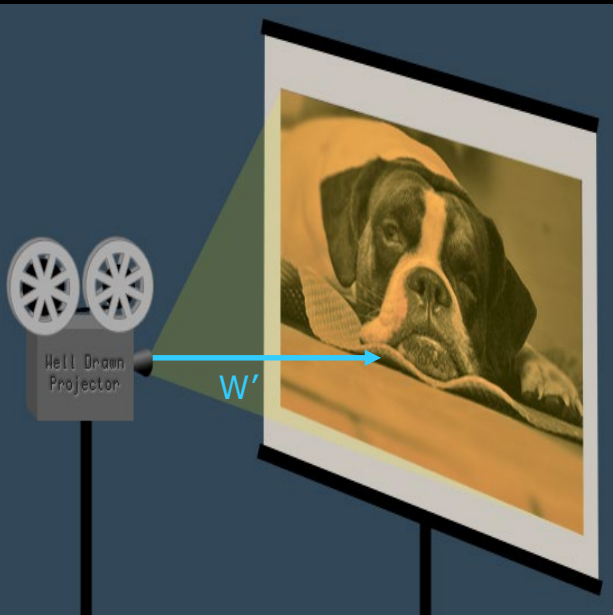
Homogeneous coordinates



- Euclidean geometry: (x, y)
 - A 2D image
 - Cartesian coordinates
- Projective geometry: (x, y, W)
 - "Projective space" adds an extra **projective** dimension, W
 - Homogeneous coordinates
 - A camera is projecting an image over a distance W .
 - *The W scales the image size:*
 (x, y, W)



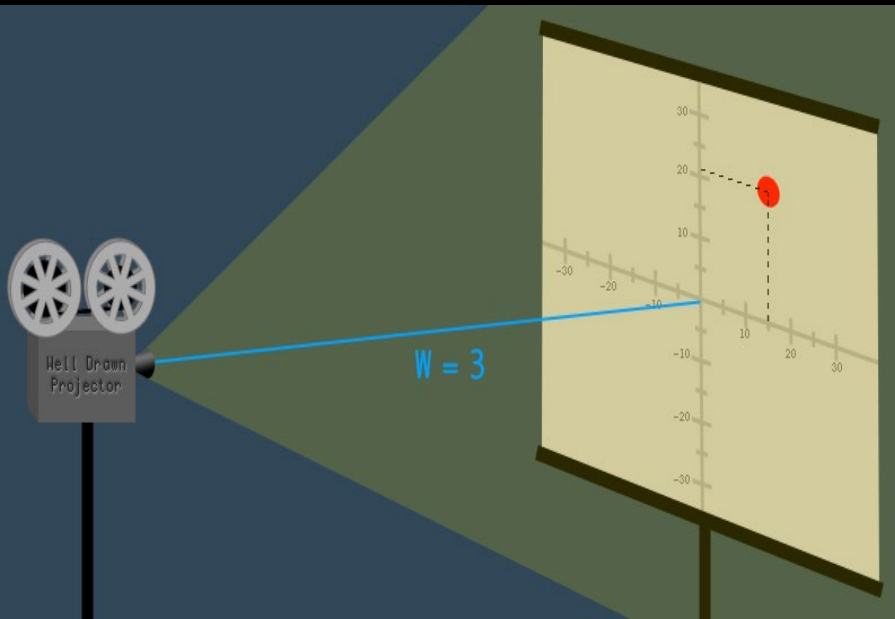
Homogeneous coordinates



- Projective geometry: (x, y, W)
 - The W *scales the image size*: (x, y, W)
 - Increasing W , the coordinates expand and the image becomes larger and vice versa
 - Decreasing relatively the distance to W' (i.e., closer) *the projective coordinate vector becomes*: $(x/W', y/W', W/W')$



Homogeneous coordinates



Example:

■ Camera:

- 3 m away from the image, $W=3$
- The **dot** on the image is at (15,21)

■ The *projective coordinate vector* is said to be

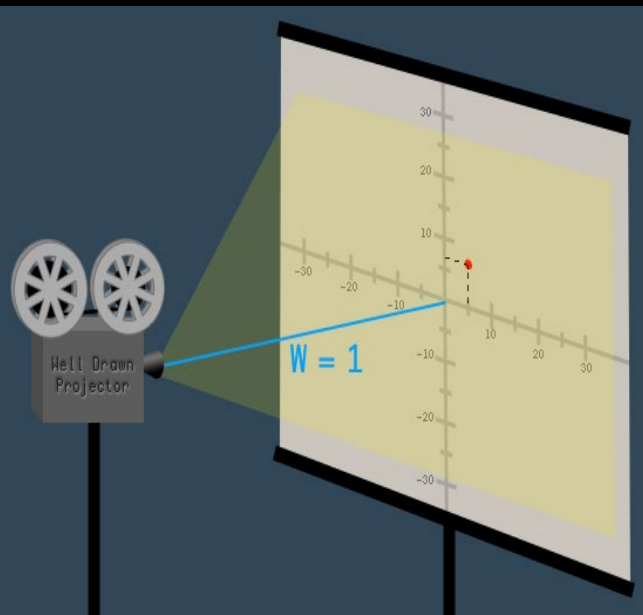
- (15, 21, 3)



Quiz 2: Homogeneous coordinates

A camera is placed at distance of 3 meter away from the image and the dot has the projective coordinate of $(15, 21, 3)$.

Now we move the camera closer to the image i.e., 1 m away. What is the new projective coordinate?



SOLUTION:

We move closer to the image i.e. W' becomes 3 times smaller and so do the projective coordinates than at $W=3$:

$$(15/3, 21/3, 3/3) = (5, 7, 1)$$

- A) $(5, 7, 1)$**
- B) $(15, 21, 3)$**
- C) $(45, 63, 1)$**
- D) $(5, 7, 0.33)$**
- E) $(0, 0, 0)$**



Translation transformation as a matrix

In Euclidian space

Translation:
$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = \begin{bmatrix} x \\ y \\ z \end{bmatrix} + \begin{bmatrix} \Delta x \\ \Delta y \\ \Delta z \end{bmatrix}$$



In Projective space

$$\begin{bmatrix} x' \\ y' \\ z' \\ W \end{bmatrix} = \begin{bmatrix} x \\ y \\ z \\ W \end{bmatrix} + \begin{bmatrix} \Delta x \\ \Delta y \\ \Delta z \\ W \end{bmatrix} \quad \text{or} \quad \begin{bmatrix} x' \\ y' \\ z' \\ W \end{bmatrix} = A_T \begin{bmatrix} x \\ y \\ z \\ W \end{bmatrix} \quad \text{where } A_T = \begin{bmatrix} 1 & 0 & 0 & \Delta x \\ 0 & 1 & 0 & \Delta y \\ 0 & 0 & 1 & \Delta z \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

■ Geometrical transformations

- Use Homogeneous coordinates
- Set $W=1$ we 'convert' 3D \rightarrow 4D space
- Translation transformation expressed as a **matrix A_T**

Transformations in Projective space

Translation:

$$A_T = \begin{bmatrix} 1 & 0 & 0 & \Delta x \\ 0 & 1 & 0 & \Delta y \\ 0 & 0 & 1 & \Delta z \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

Rotations:

- x=pitch
- y=roll
- z=yaw

$$R_x = \begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & \cos(\alpha) & \sin(\alpha) & 0 \\ 0 & -\sin(\alpha) & \cos(\alpha) & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

$$R_y = \begin{bmatrix} \cos(\beta) & 0 & \sin(\beta) & 0 \\ 0 & 1 & 0 & 0 \\ -\sin(\beta) & 0 & \cos(\beta) & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

$$R_z = \begin{bmatrix} \cos(\gamma) & \sin(\gamma) & 0 & 0 \\ -\sin(\gamma) & \cos(\gamma) & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

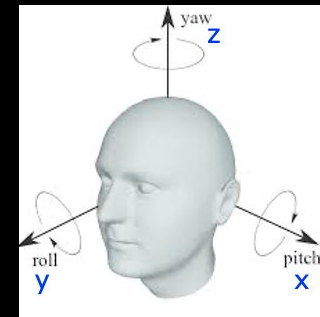
Scaling:

$$A_s = \begin{bmatrix} S_x & 0 & 0 & 0 \\ 0 & S_y & 0 & 0 \\ 0 & 0 & S_z & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

Shear:

$$A_z = \begin{bmatrix} 1 & S_{xy} & S_{xz} & 0 \\ S_{xy} & 1 & S_{yz} & 0 \\ S_{xz} & S_{yz} & 1 & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

- Axis-Angle representation



Affine transformation: $A = A_T * \underbrace{(R_x * R_y * R_z)}_{\text{Rigid}} * A_z * A_s$

Rigid



Combining transformations – step by step

Remember:

- Typical calculated in *radians*
- *Same procedure for 2D and 3D images*

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = \begin{bmatrix} x \\ y \\ z \end{bmatrix} + \begin{bmatrix} \Delta x \\ \Delta y \\ \Delta z \end{bmatrix}$$

- Step 1: Convert 3D to 4D projective space, set $W=1$. Make translation into a matrix

$$A = A_T * (R_x * R_y * R_z) * A_z * A_s \quad \text{▪ Step 2: Multiply all 4D matrices}$$

$$\begin{bmatrix} x' \\ y' \\ z' \\ 1 \end{bmatrix} = A \cdot \begin{bmatrix} x \\ y \\ z \\ 1 \end{bmatrix}$$

- Step 3: Apply the transformation to a point

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = A \cdot \begin{bmatrix} x \\ y \\ z \end{bmatrix}$$

- Step 4: Convert back to 3D Cartesian coordinates by ignoring the W dimension



Different transformations

- Linear: Affine transformation
- Non-linear: Piece-wise affine or B-spline
 - Remember: First to apply the linear transformations!

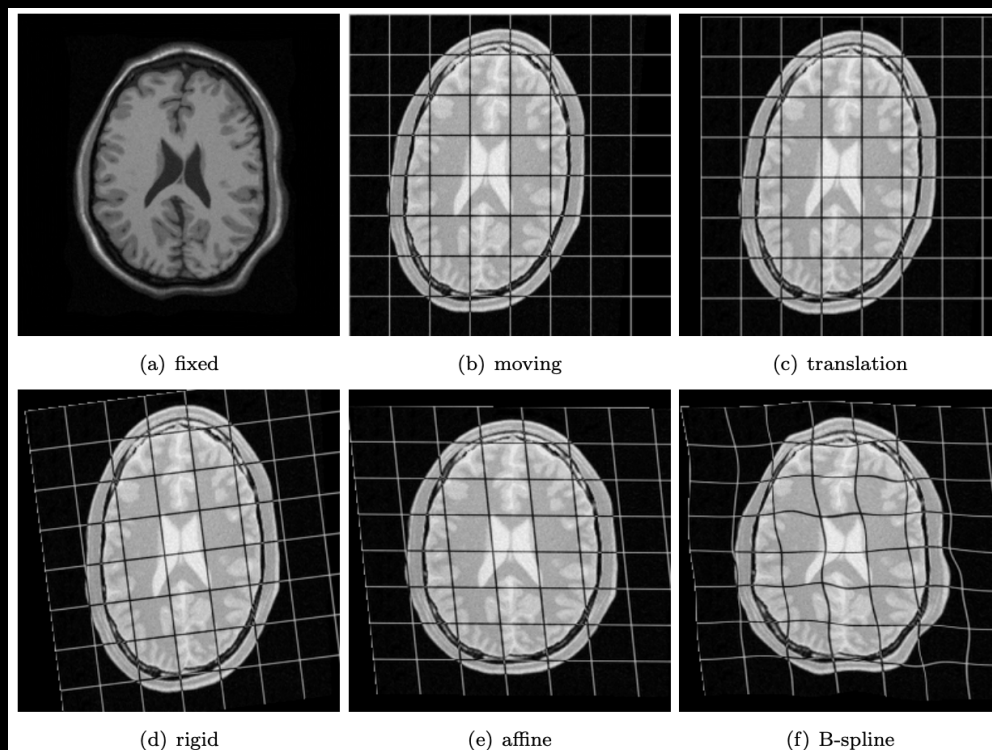
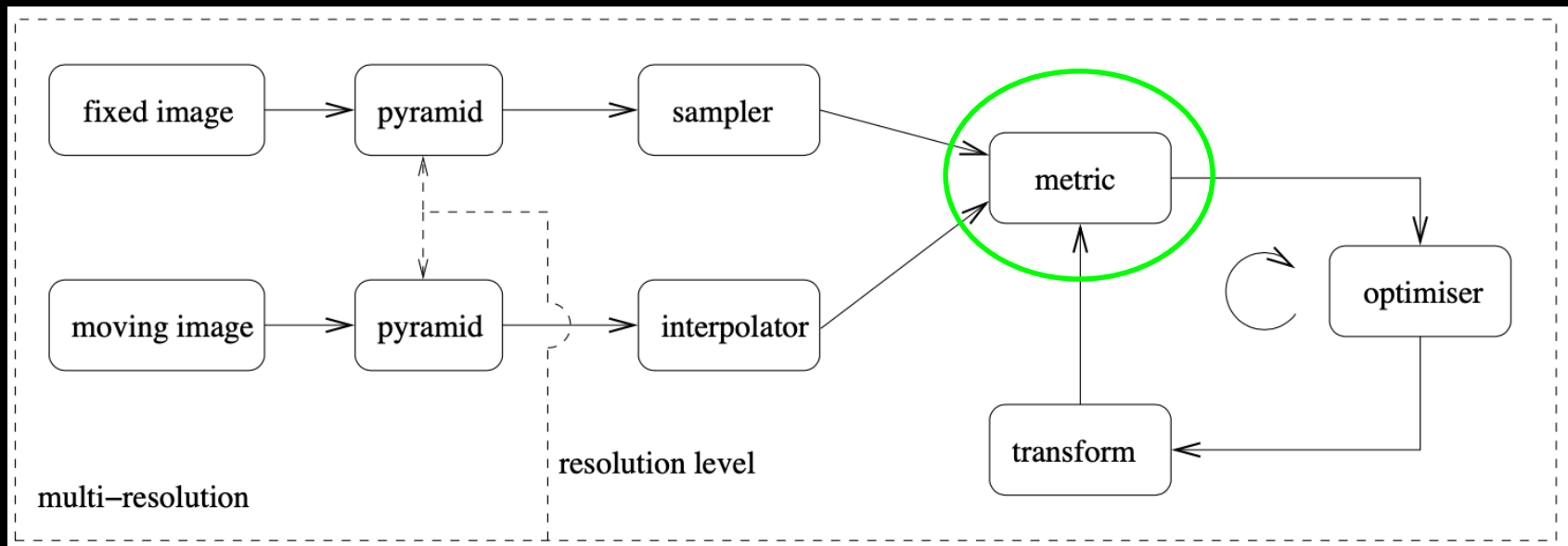


Image Registration pipeline

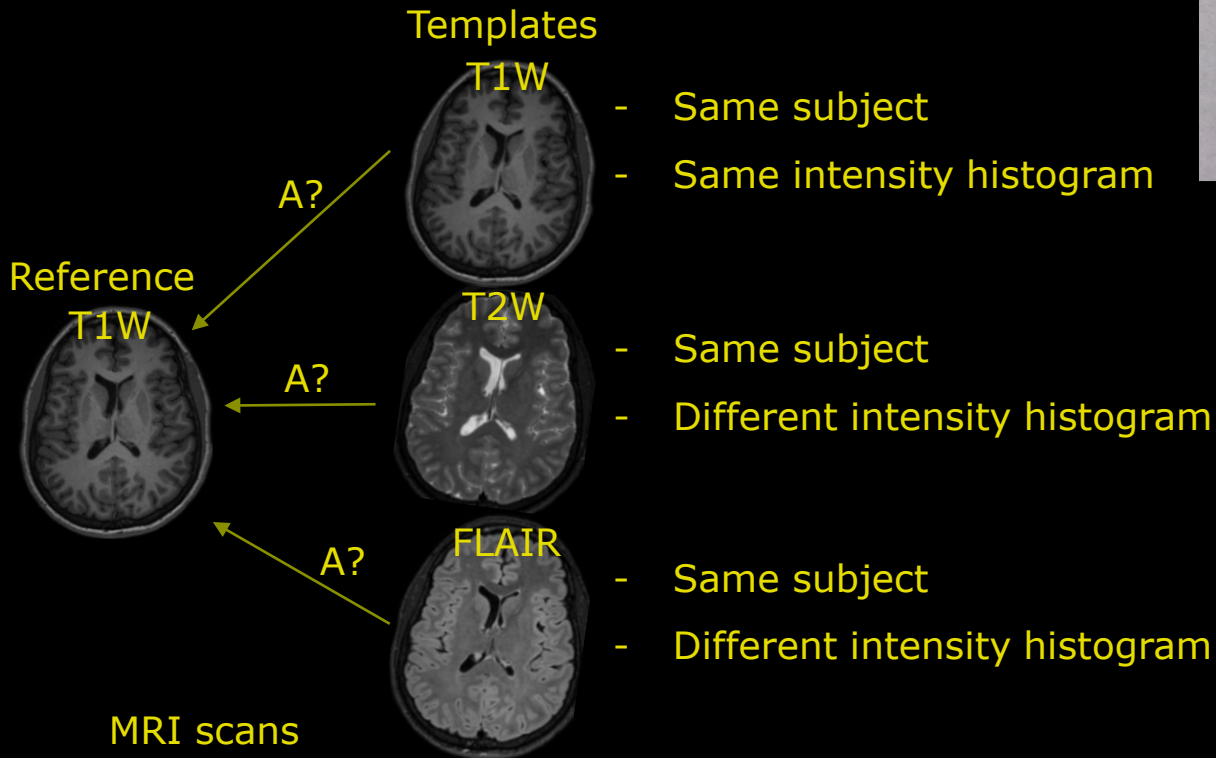
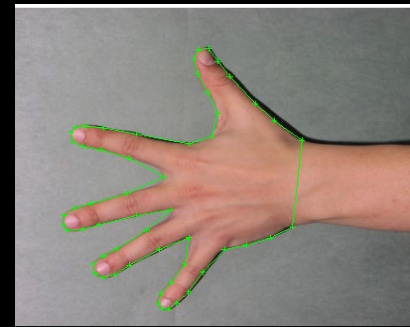
■ Similarity measures



Similarity measures

■ Anatomical Landmarks

- time consuming to obtain positions manually
- Alternative: **Joint intensity histogram**





Similarity measure: Mean squared difference (MSD)

- Compare difference in intensities.
 - Same similarity measure we used for anatomical landmarks (positions) in a previous lecture
 - Super fast to estimate
- Many local minima's (sub optimal solutions)
 - Intensities are not optimal for this similarity metric

$$\text{MSD}(\boldsymbol{\mu}; I_F, I_M) = \frac{1}{|\Omega_F|} \sum_{\mathbf{x}_i \in \Omega_F} (I_F(\mathbf{x}_i) - I_M(\mathbf{T}_{\boldsymbol{\mu}}(\mathbf{x}_i)))^2,$$



Similarity measure: Normalised Cross-correlation

- Normalised Cross-correlation of intensities in two images
 - Fast to estimate
- Risk of local minima's (sub optimal solutions)
 - Less robust if image modalities have different intensity histograms
 - Normalise: Reduce the impact of outlier regions

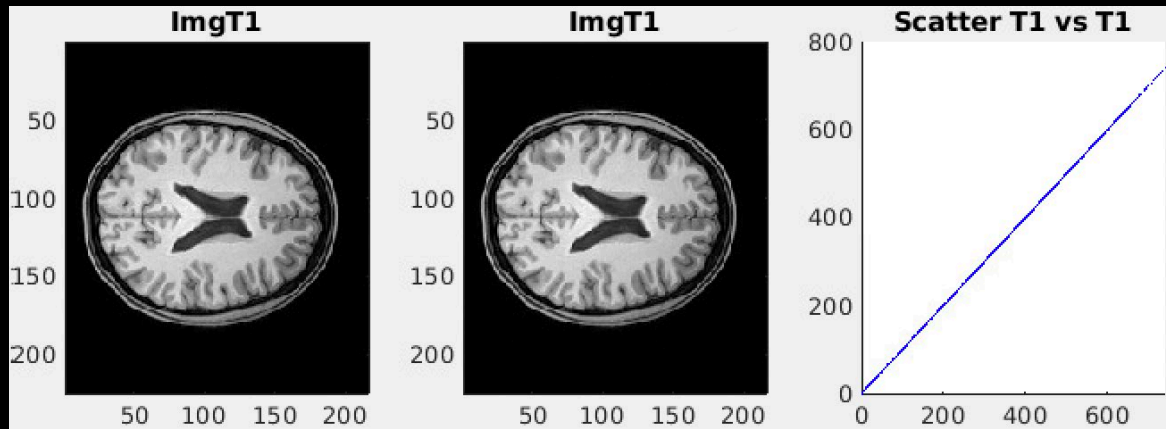
$$\text{NCC}(\boldsymbol{\mu}; I_F, I_M) = \frac{\sum_{\mathbf{x}_i \in \Omega_F} (I_F(\mathbf{x}_i) - \bar{I}_F) (I_M(\mathbf{T}_{\boldsymbol{\mu}}(\mathbf{x}_i)) - \bar{I}_M)}{\sqrt{\sum_{\mathbf{x}_i \in \Omega_F} (I_F(\mathbf{x}_i) - \bar{I}_F)^2 \sum_{\mathbf{x}_i \in \Omega_F} (I_M(\mathbf{T}_{\boldsymbol{\mu}}(\mathbf{x}_i)) - \bar{I}_M)^2}},$$

with the average grey-values $\bar{I}_F = \frac{1}{|\Omega_F|} \sum_{\mathbf{x}_i \in \Omega_F} I_F(\mathbf{x}_i)$ and $\bar{I}_M = \frac{1}{|\Omega_F|} \sum_{\mathbf{x}_i \in \Omega_F} I_M(\mathbf{T}_{\boldsymbol{\mu}}(\mathbf{x}_i))$.

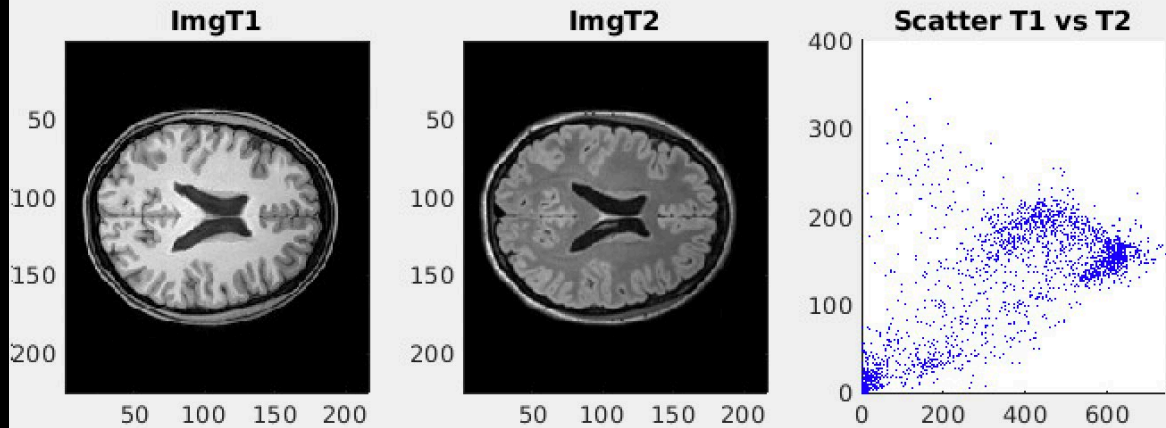
Joint intensity histograms

- Perfect registered: Optimal joint intensity agreement

Same image modality



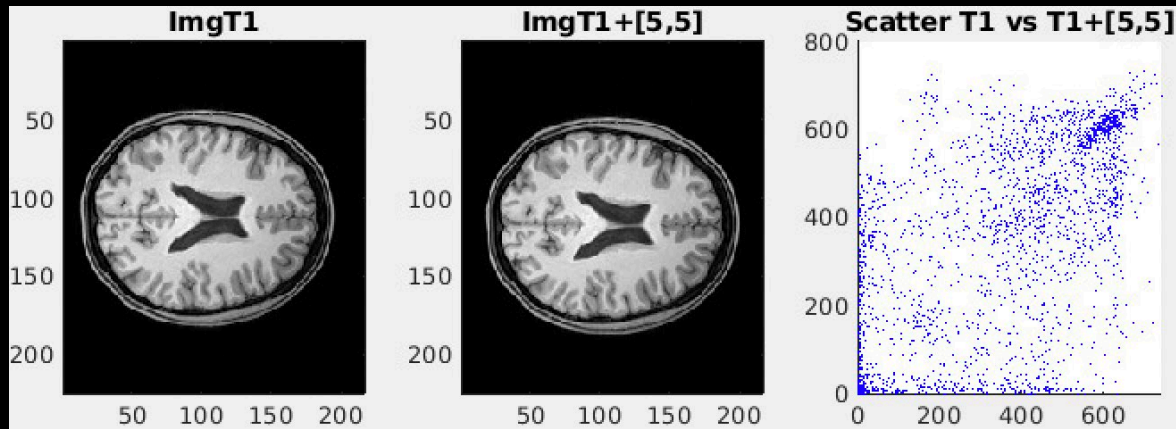
Different image modality



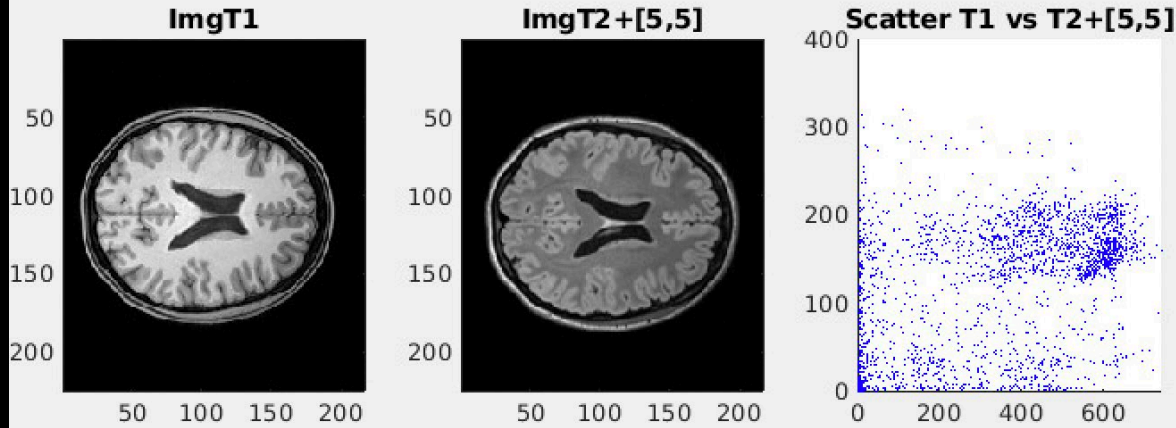
Joint intensity histograms

- Small translation difference: Lower joint intensity agreement

Same image modality



Different image modality





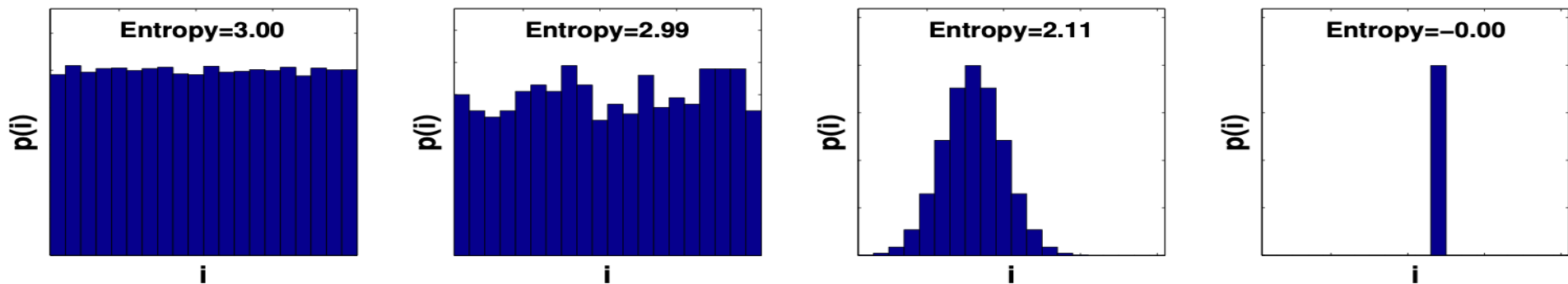
Similarity measure - Entropy

- Comes from information theory.
 - The higher the entropy the more the information content.
- Entropy (Shannon-Weiner):

$$H = -\sum_i p_i \log_b p_i$$

Where b : the base of the logarithm

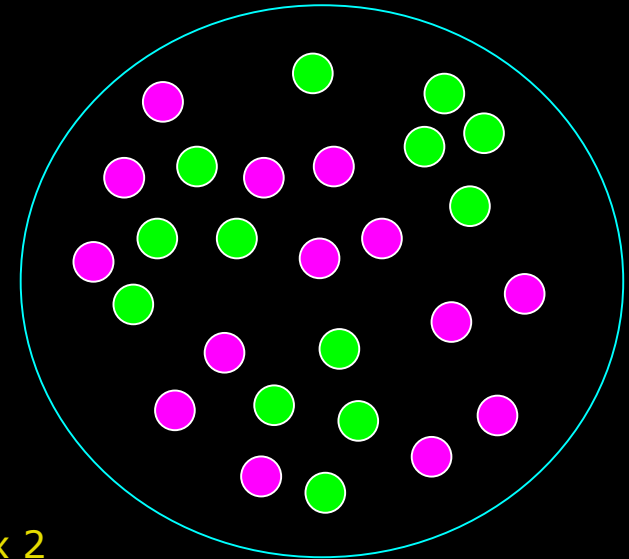
- Bits: $b=2$ and bans: $b=10$
- Entropy is typically in bits i.e. typical used in digital information



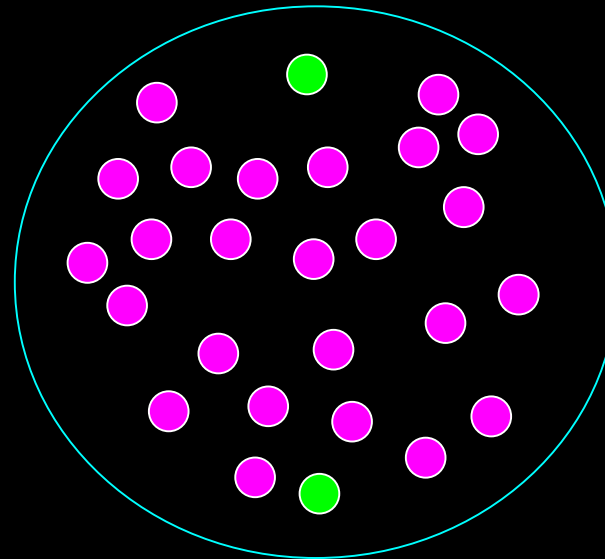


Quiz 3: Highest entropy?

I went to the candy shop and wanted to select the candy mixture that have the highest entropy. Each candy mixture include in total 27 pieces. Which one should I select?



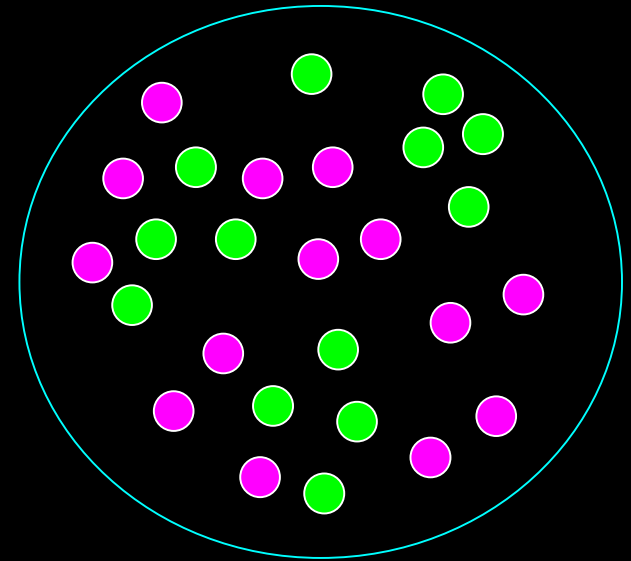
Candy mix 2



- A) Mix 1
- B) Make a new choice
- C) Contain no liquorice
- D) Mix 2
- E) It is not healthy

Quiz 4: What is the entropy of the candy mix 1?

Candy mix 1



A) 0.38

B) 0.99

C) 0.45

D) 0.23

E) 0.00

SOLUTION:

Green=13

Pink=14

Total=27

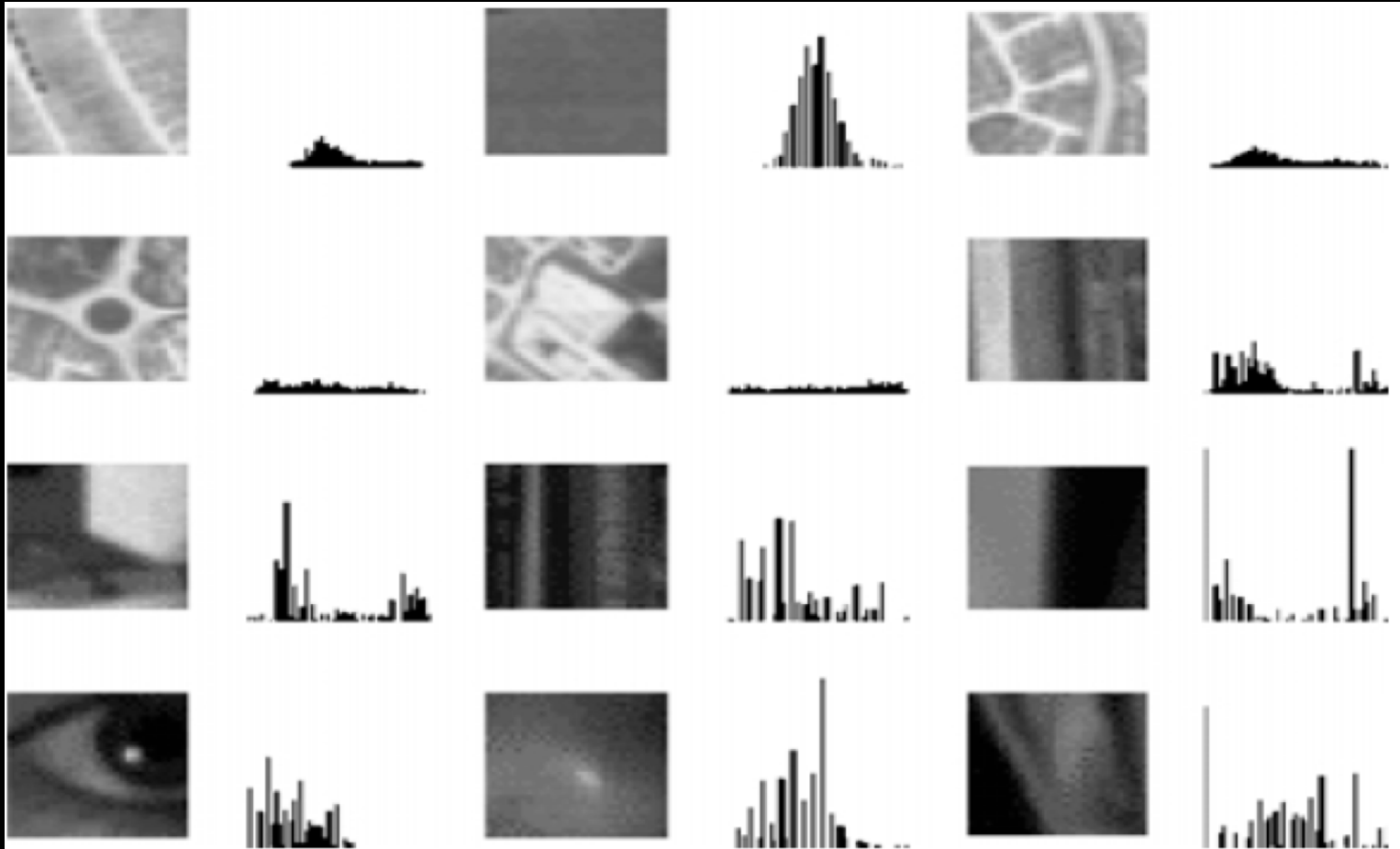
$p_G = 13/27$

$p_P = 14/27$

Entropy = $-p_G \cdot \log_2(p_G) - p_P \cdot \log_2(p_P) = 0.99$



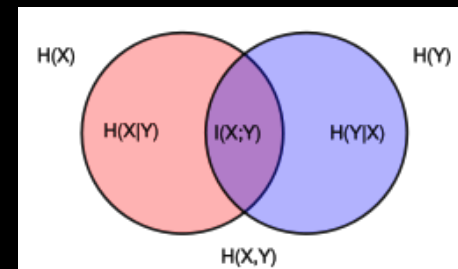
Histograms of images



Joint entropy - Mutual information

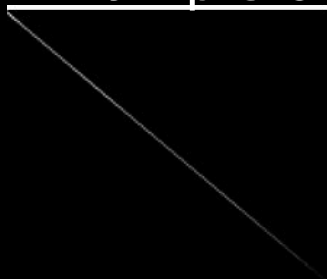
- Joint entropy $H = - \sum_{X,Y} p_{X,Y} \log p_{X,Y}$
- Similarity measure: The more similar the distributions, the lower the joint entropy compared to the sum of the individual entropies

$$H(X,Y) \leq H(X) + H(Y)$$



en.wikipedia.org/wiki/Mutual_information

- Example of rotation (Pluim et al., 2003, TMI)



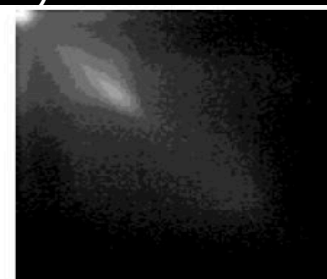
3.82

0 degrees



6.79

2 degrees



6.98

5 degrees



7.15

10 degrees





Contrast in joint histograms

- The histogram of the two images must reflect contrast to similar structures for image registration to be successful

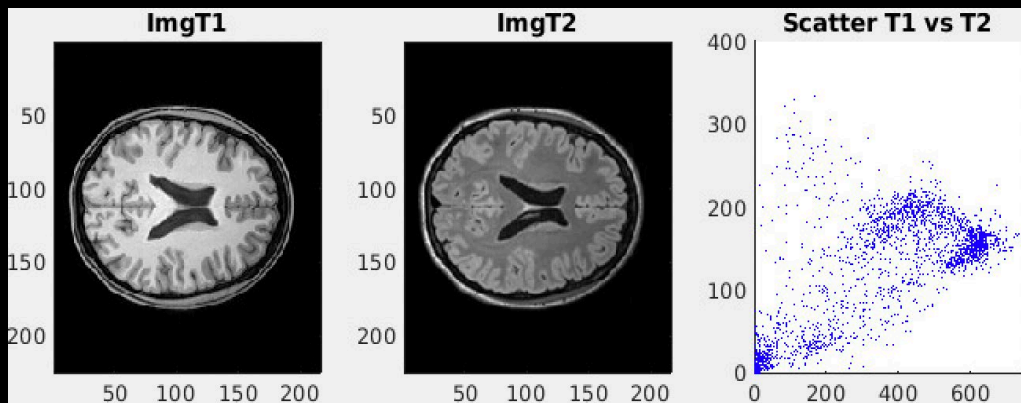
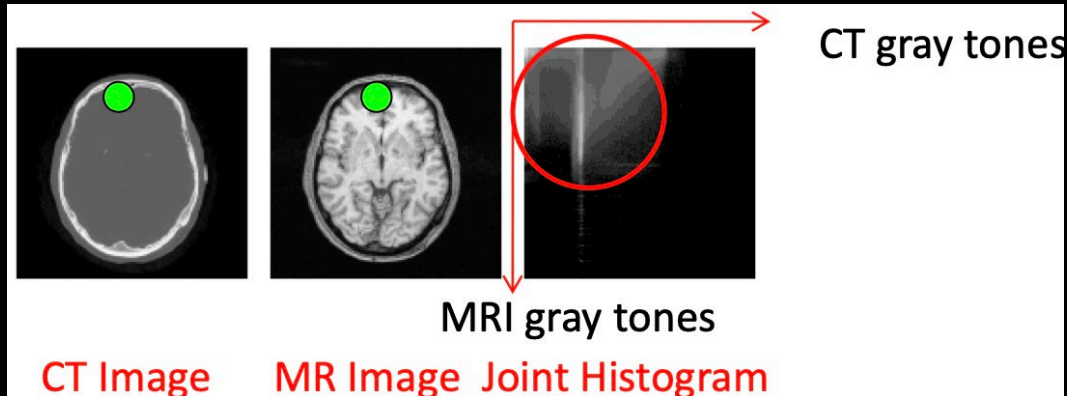
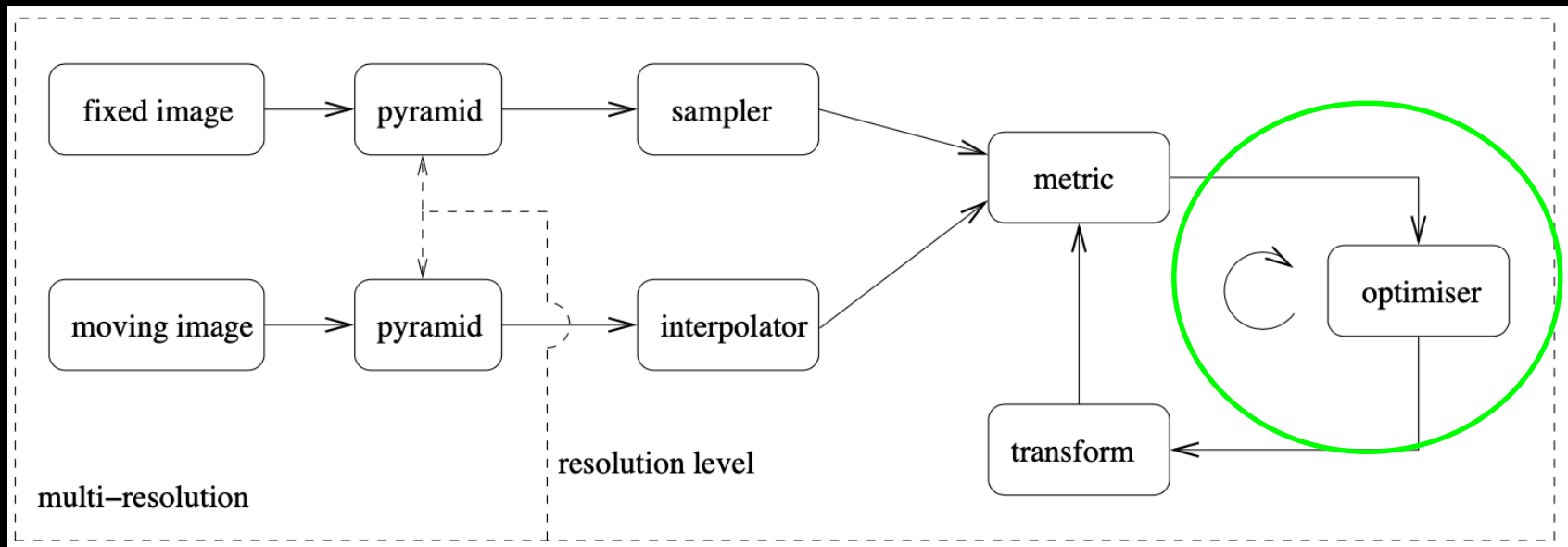


Image Registration pipeline

■ The optimiser

- How to find the transformation parameters?





The optimizer

- We have an **objective function** describing:
 - A **cost function (C)** based on a **similarity metric**
 - Quantifying how well a **geometrical transformation** ($T(w)$) maps an image (moving, I_M) into another (fixed, I_F)
- Hence, a good match is a minimum difference:

$$\hat{T}_w = \arg \min_{T_w} C(T_w; I_F, I_M)$$



The parameters

$$w \in \mathcal{R}^p$$

- The parameters is a vector with p elements
- The type of transformation and the dimension of the dataset set the number of parameters
 - Translation $p = 2$ or 3 (3D)
 - Rotation $p = 1$ or 3 (3D)
 - Scaling $p = 1$



Optimization by minimization

- Find the parameter set that minimizes the objective function
- How to find the solution?
 - Analytical: Works fine for landmark registration with few points
 - Numerical: Iterative approaches to search for a solution

To find: $\hat{w} = \arg \min_w C$

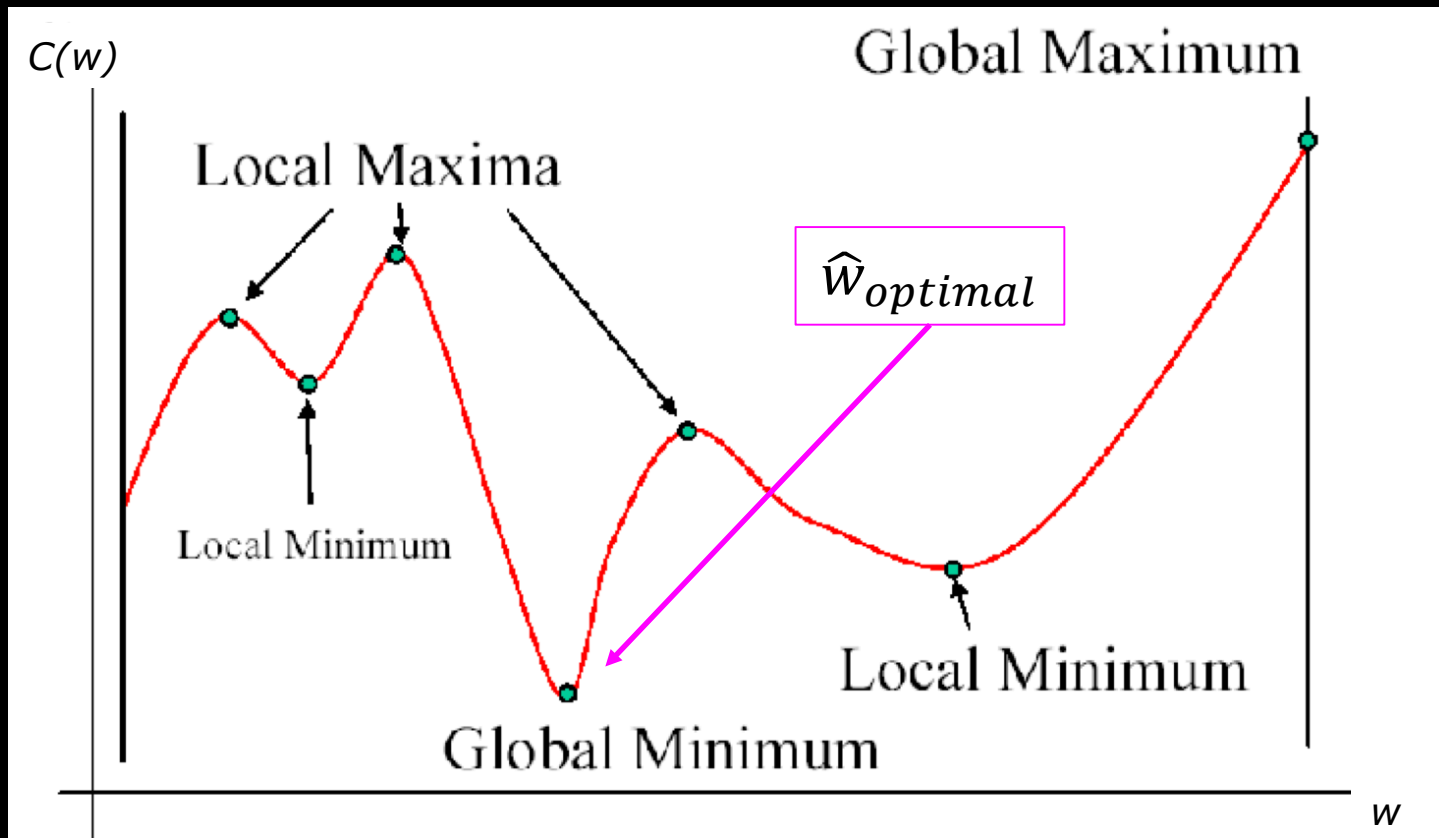
We simply differentiate w.r.t. w :

$$\frac{\partial C}{\partial w} = 0$$



The challenge

- \mathbf{w} span a p -dimensional space $\mathbf{w} = [w_1, w_2, \dots, w_p]^T$
- Complex parameter space with many data points
 - Finding the lowest place in mountains



Iterative optimisation

- Aim: Find in parameter space w : $\frac{\partial C}{\partial w} = 0$ i.e. a global minima
 - Search all possible combinations of w ? (not a good idea)
 - Systematically search the parameter space = Good idea

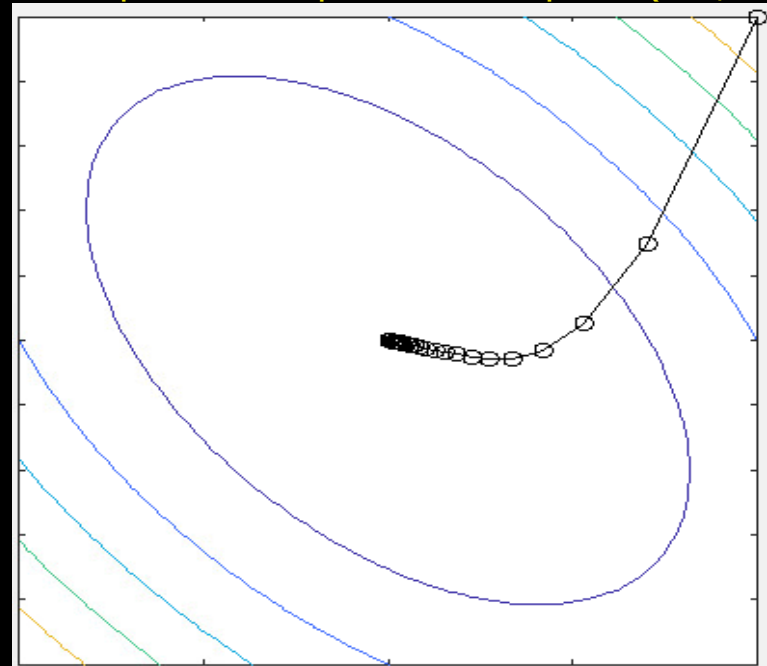
- Iterative optimisation strategies

- Step-wise searching the parameter space

- Many methods exist

- Gradient based
- Genetic evolution
- ...

Contour plot of 2D parameter space (w_1, w_2)

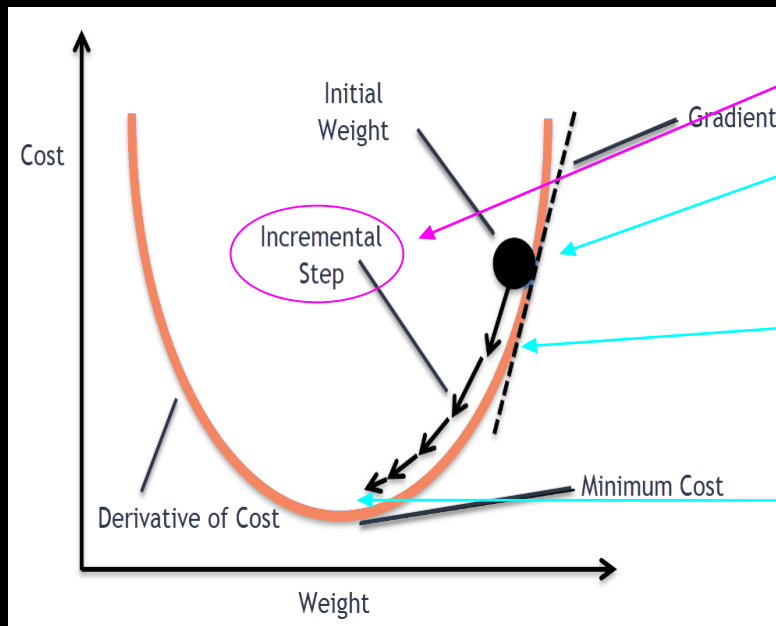


Gradient descent

- Definition: $C(\mathbf{w})$ is differentiable in neighbourhood of a point w_n
- $C(\mathbf{w})$ decreases in the *negative* gradient direction of w_n .
- $w_{n+1} = w_n - \gamma \nabla C(w_n)$
 - $\nabla C(w_n)$: Gradient direction at point w_n
 - γ : Step length --> If small enough: $C(w_n) \geq C(w_{n+1})$

Procedure:

- 0) Define a step length γ
- 1) Start guess of a position w_0
- 2) Find gradient
- 3) Take a step
- 4) Repeat 2)+3)
- 5) Solution: Global minima



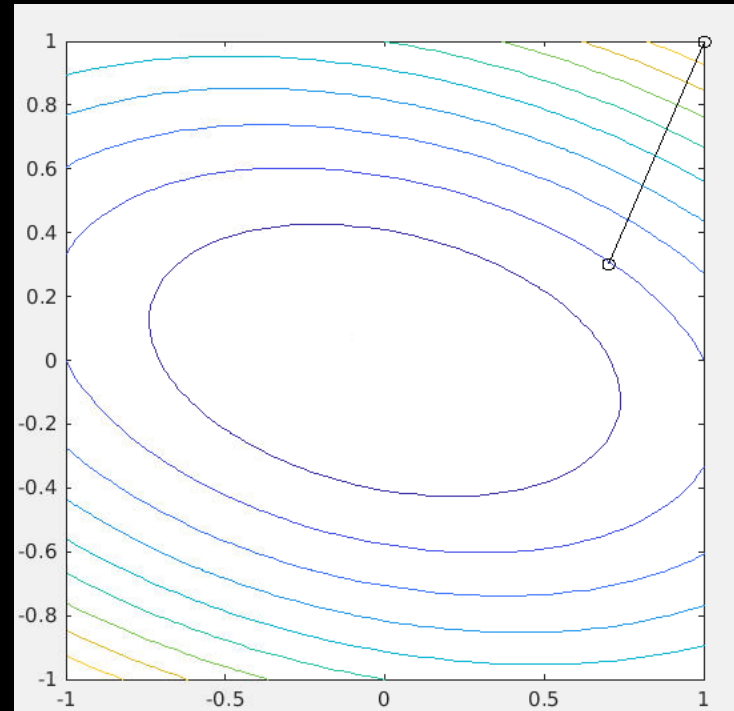
$$\nabla C(w_{n+1}) = \frac{\partial C}{\partial w} \approx 0$$



Gradient descent

- Cost function: $C(\mathbf{x}) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$;
- Max steps: 1000
- Start position: $\mathbf{x}_0=[1,1]^T$

Iteration: 1



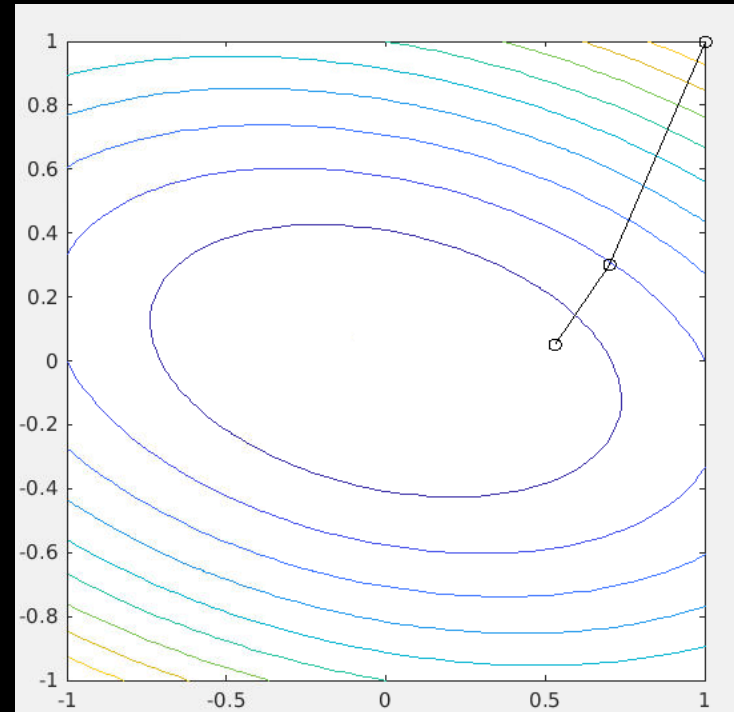
From a Matlab function: *grad_descent.m*
By James T. Allison



Gradient descent

- Cost function: $C(\mathbf{x}) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$;
- Max steps: 1000
- Start position: $\mathbf{x}_0=[1,1]^T$

Iteration:2

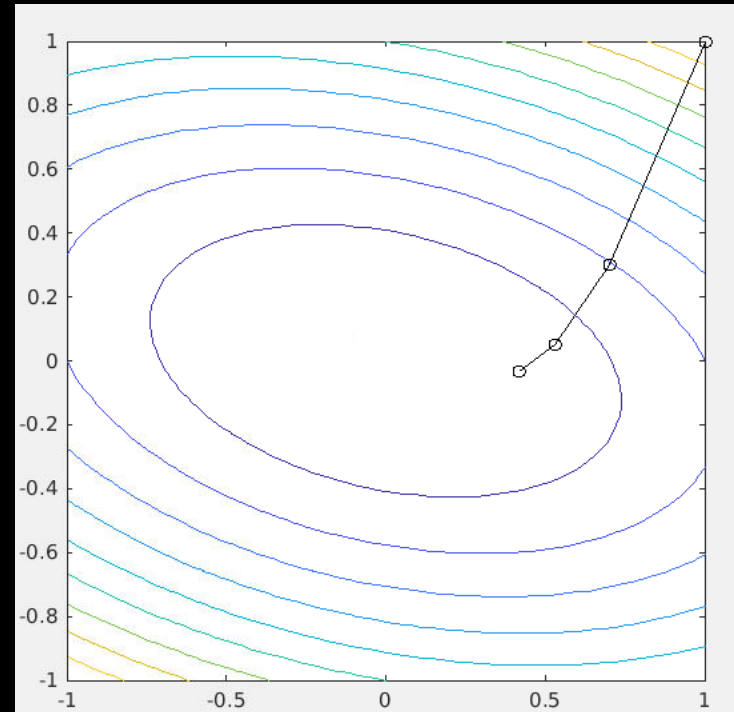




Gradient descent

- Cost function: $C(\mathbf{x}) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$;
- Max steps: 1000
- Start position: $\mathbf{x}_0=[1,1]^T$

Iteration:3

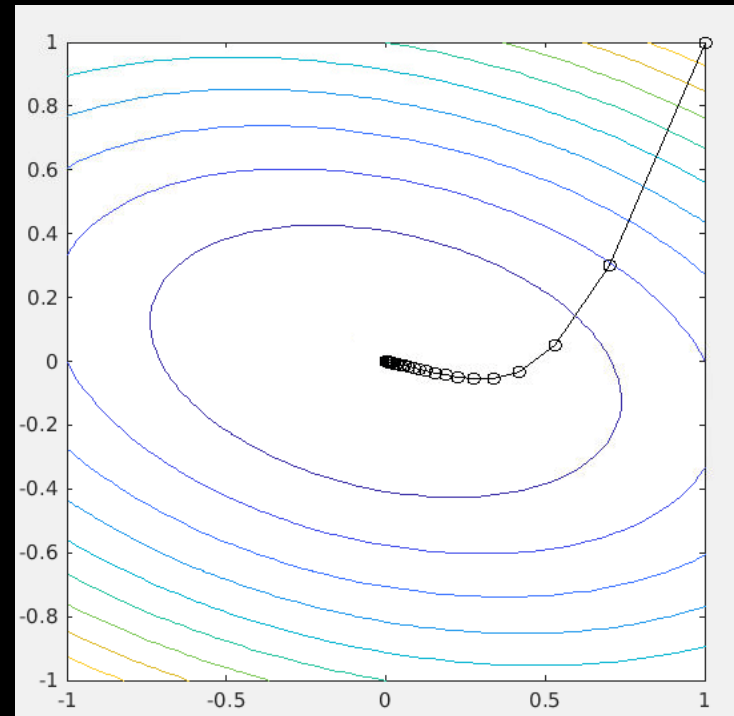




Gradient descent

- Cost function: $C(\mathbf{x}) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$;
- Max steps: 1000
- Start position: $\mathbf{x}_0=[1,1]^T$

Iteration: 37 (final)

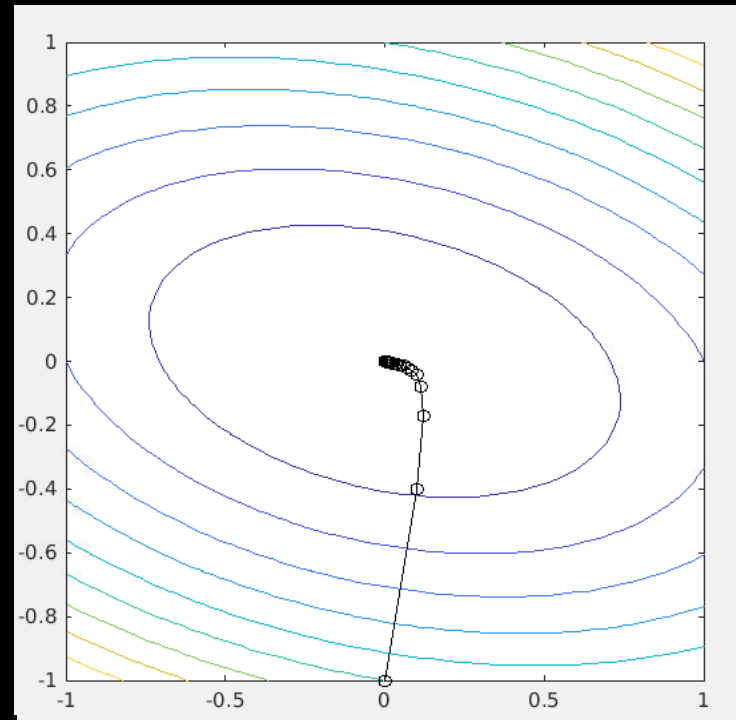




Gradient descent

- Cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = - \begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$;
- Max steps: 1000
- Start position: $x_0=[0,-1]^T$
- Can find solution from any place
- No local minima's nearby

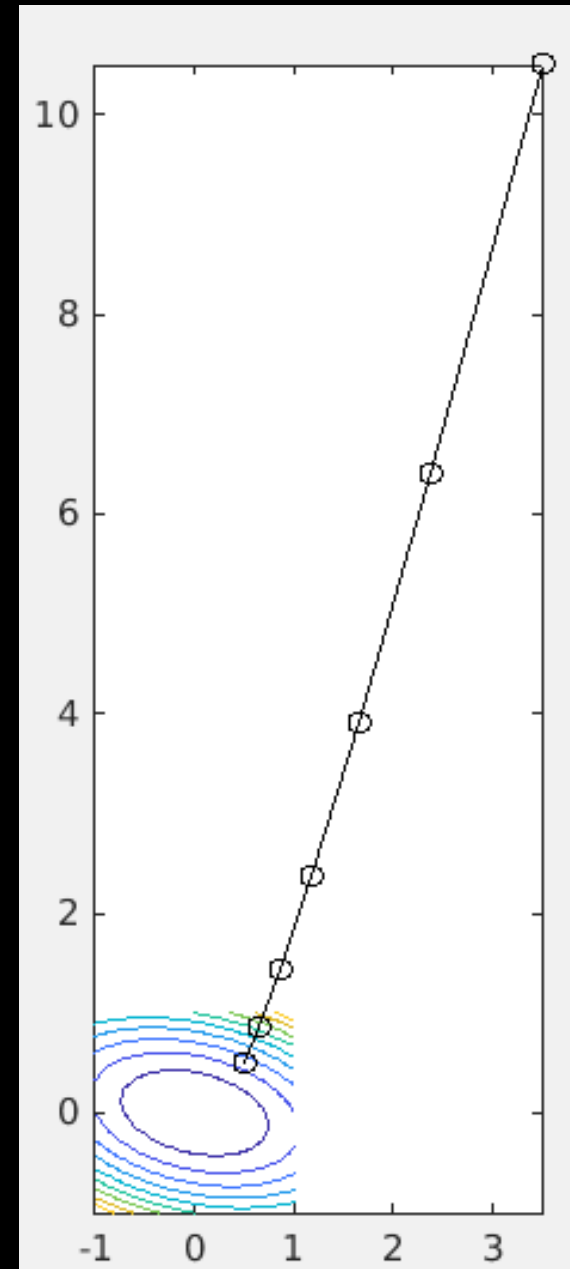
Iteration: 31 (final)





Gradient descent

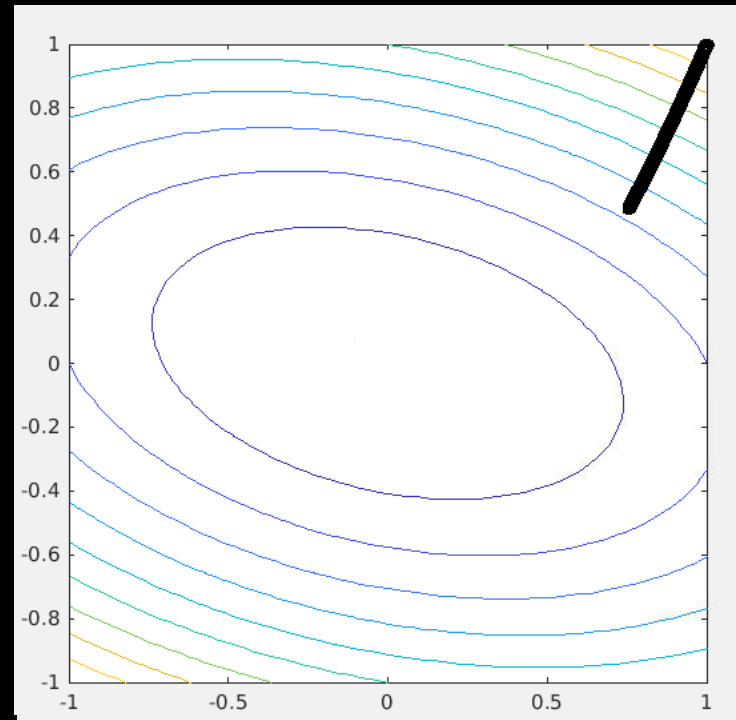
- Cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $+\nabla C(x_n) = + \begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$;
- Max steps: 1000
- Start position: $x_0=[0.5,0.5]^T$
- If use positive gradient
 - WRONG DIRECTION!



Gradient descent

- Cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.0001$;
- Max steps: 1000
- Start position: $x_0=[1,1]^T$
- Too small step size –many steps
- Do not find a solution

Iteration:1000 (final)

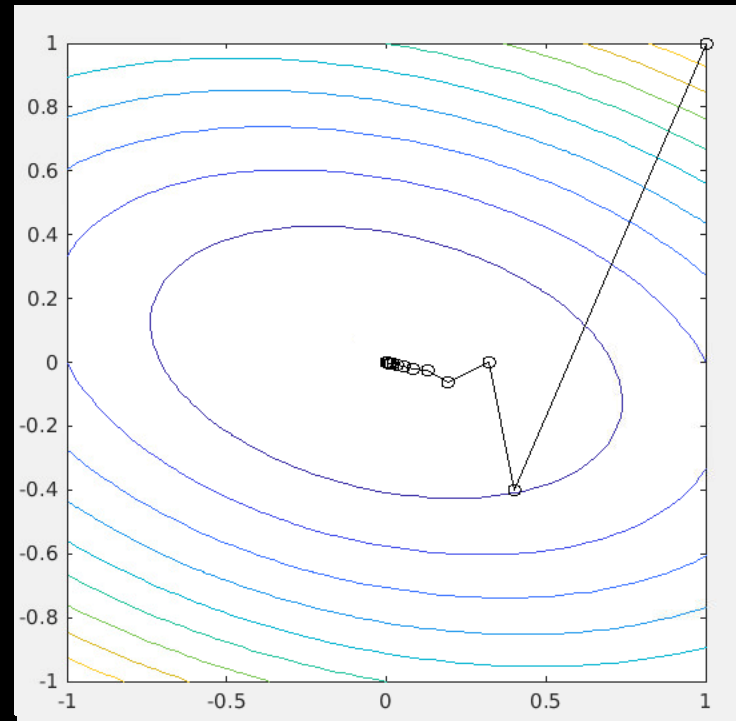




Gradient descent

- Cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = - \begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.2$ (optimal)
- Max steps: 1000
- Start position: $x_0=[1,1]^T$
- Few steps: Optimal step size

Iteration: 17 (final)

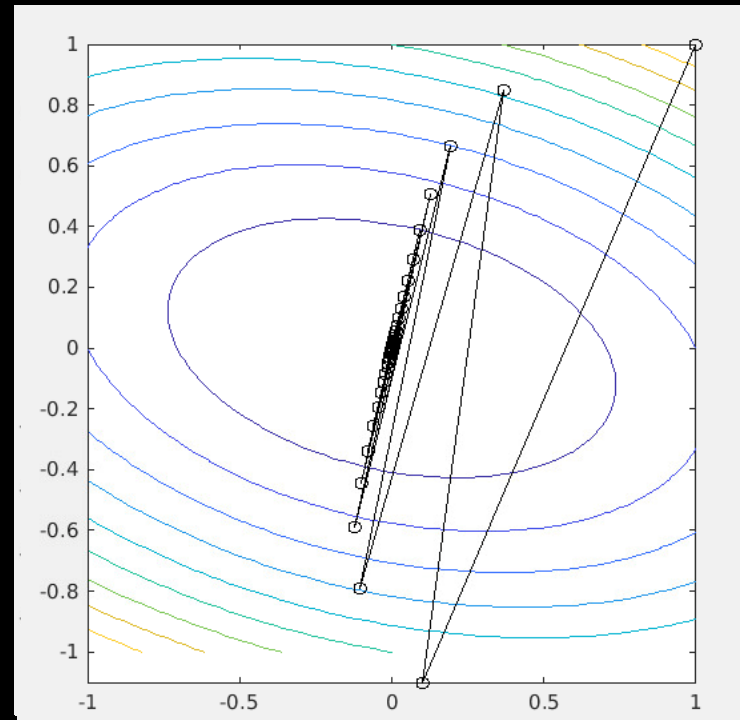




Gradient descent

- Cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.3$
- Max steps: 1000
- Start position: $x_0=[1,1]^T$
- Too large step size – unstable
- Sensitive to local minima's
- Solution: Dynamic step length

Iteration:65 (final)

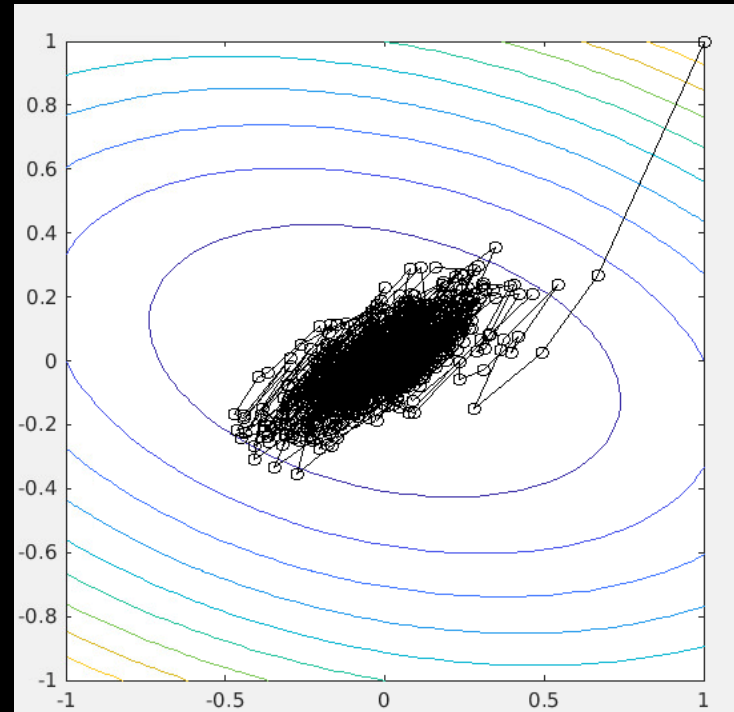




Gradient descent

- Cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
- Gradient at point x_n : $-\nabla C(x_n) = -\begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$
- Step length: $\gamma=0.1$
- Max steps: 1000
- Start position: $x_0=[1,1]^T$
- Noisy data: Cannot find optimum

Iteration: 1000 (final)





Quiz 5: What is the updated position x_{new} ?

Model fitting uses a cost function: $C(x) = x_1^2 + x_1x_2 + 3x_2^2$
and an iterative optimizer Gradient descent with a step length of 0.2

What is the new position of $x_{new} = [?, ?]^T$ after one step from position $x = [1, 0]^T$?

- A) $[0.3, 2.3]^T$
- B) $[-1.7, 0.3]^T$
- C) $[1.4, 0.2]^T$
- D) $[0.6, -0.2]^T$**
- E) $[5.2, 2.2]^T$

Solution:

1) Calculate the gradient for $x = [1, 0]^T$

- differentiate C: $\nabla C(x) = \begin{bmatrix} 2x_1 + x_2 \\ x_1 + 6x_2 \end{bmatrix}$

$$\nabla C([1, 0]^T) = [2, 1]^T$$

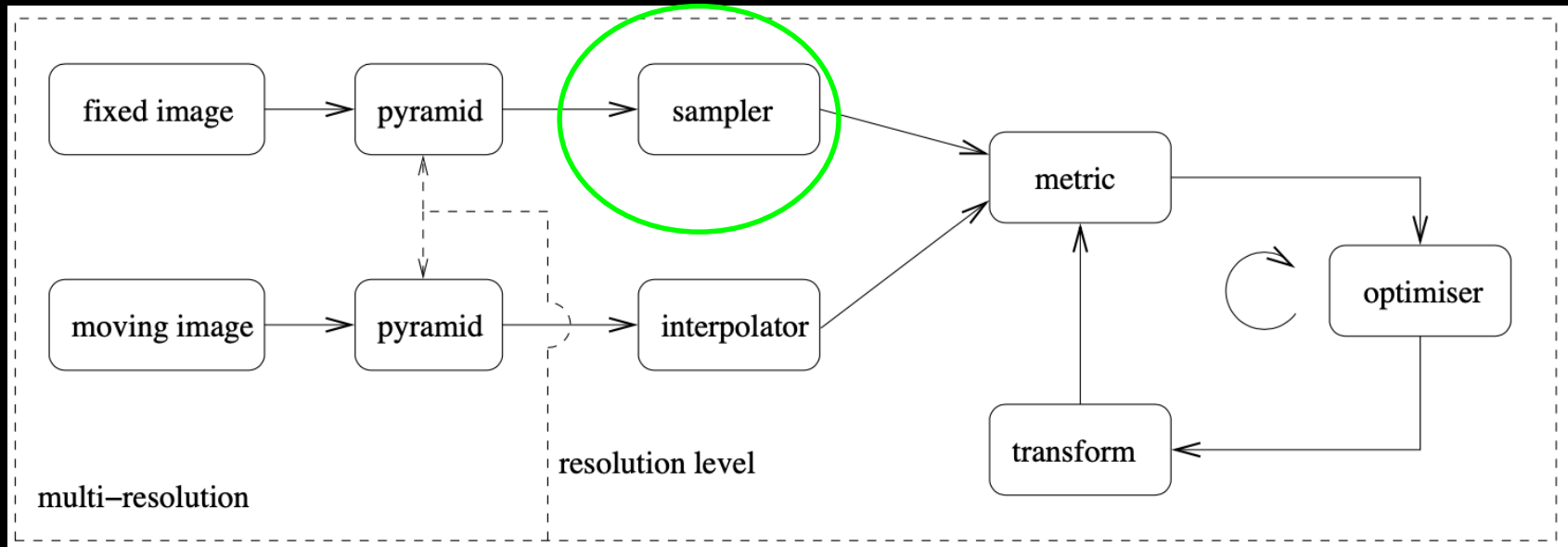
2) Update the step: $x_{new} = x - \nabla C * \text{stepLength}$

- $x_{new} = [1, 0]^T - 0.2 * [2, 1]^T = [0.6, -0.2]^T$

Image Registration pipeline

■ The sampler

- How many data points for a robust similarity measure?





The sampler

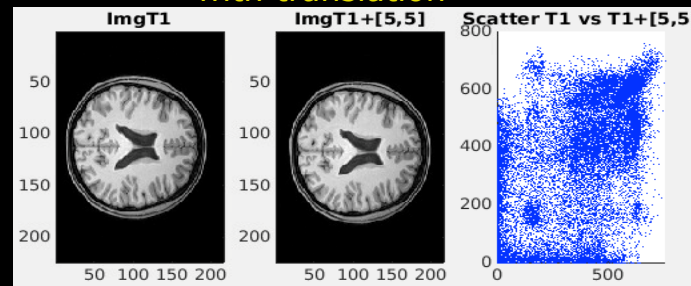
- Calculating the similarity metrics:
 - Summing over all pixels/voxels in an image is VERY time consuming
- Selecting a sparse sampling strategy
 - Reducing CPU load and reduce memory load when
 - Efficient selection of image points



The sampler

- Sparser sampling: Similar scatter plot
 - Define a good compromise (sample the whole image)
- Ordered vs Random
 - Spatial dependency: Dependent on large homogeneous structures
 - Very sparse sampling: Risk not sampling small structures

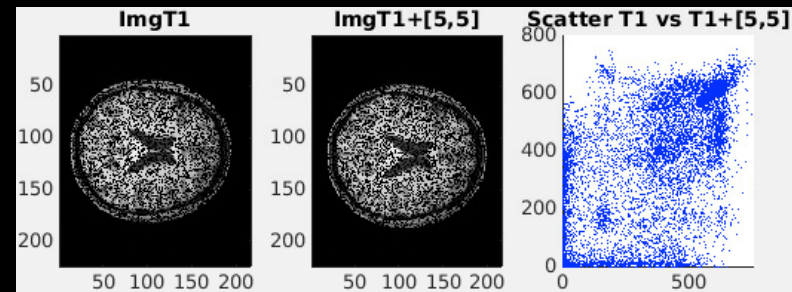
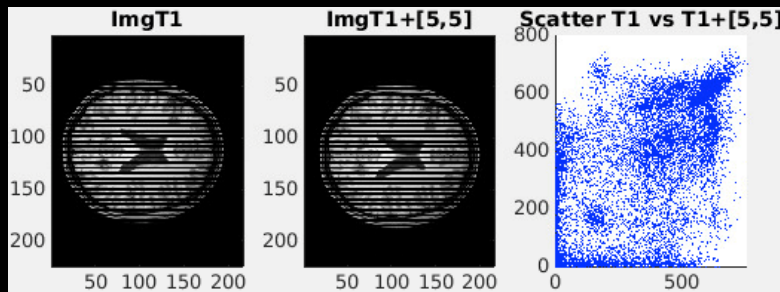
All samples



Ordered

Random

Every 2nd



Every 10th

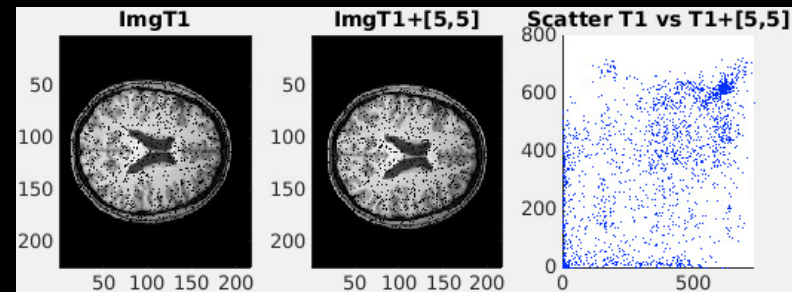
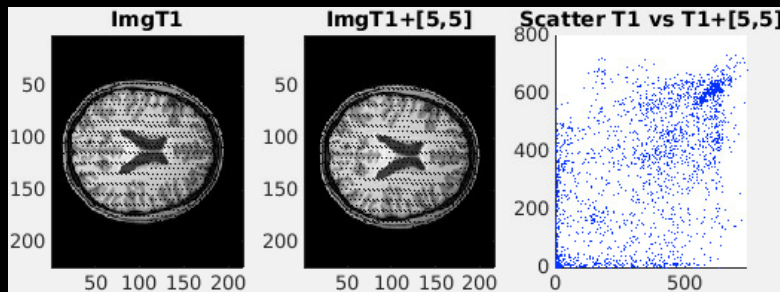
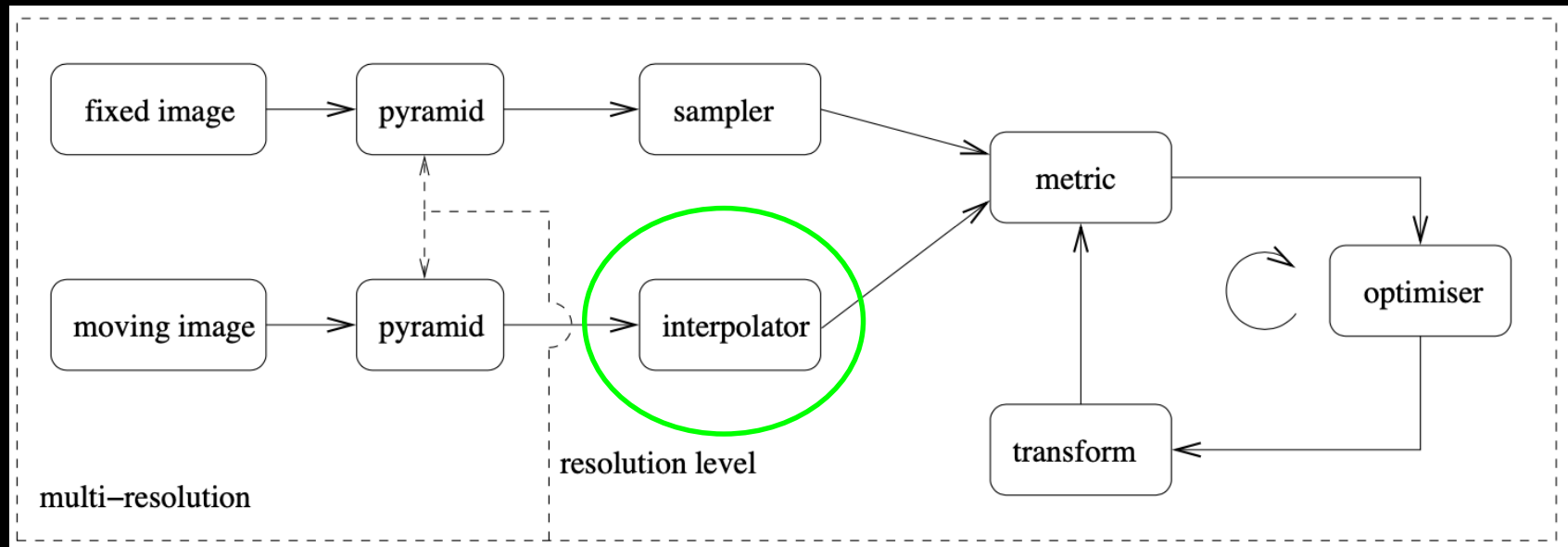


Image Registration pipeline

■ Interpolation

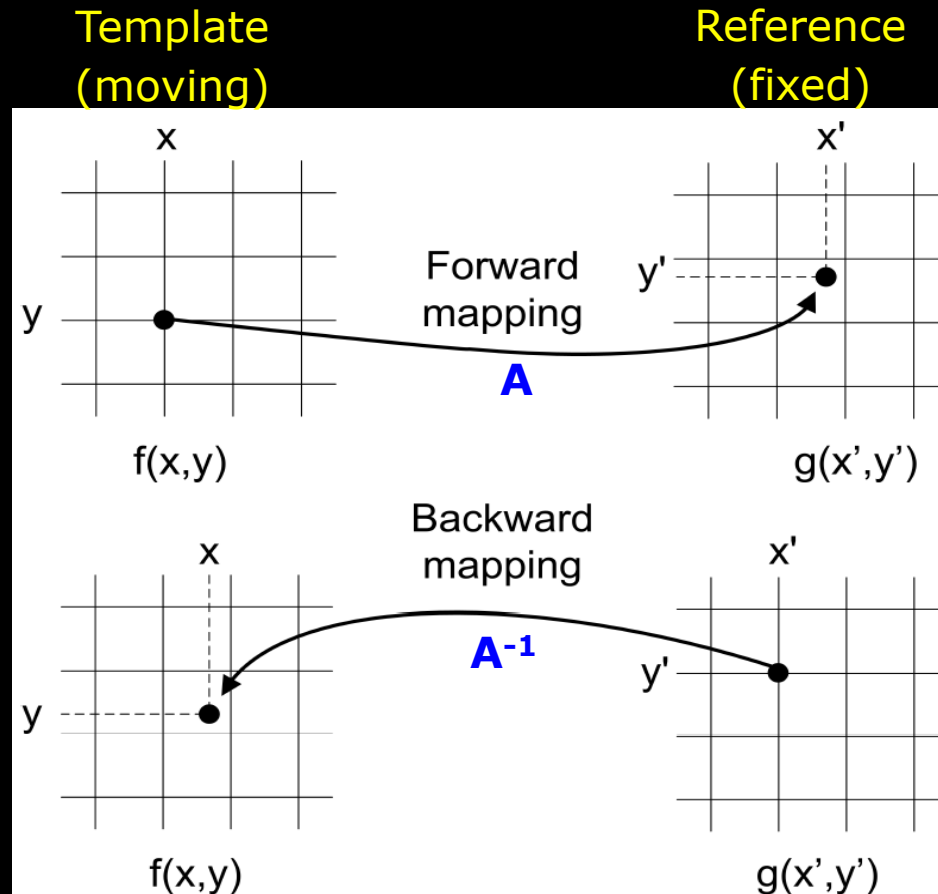
- To map the intensities from the template image to the grid of the reference image via a transformation matrix





A FLASH BACK to a previous Lecture: Forward vs Backward mapping

- In a nut shell
 - Going backward we need to invers the transformation



Interpolation methods

- Enhances structural boundaries
 - Higher-order interpolation methods: Reduce blurring
- May visually appear “sharper”
 - Do not change the image information!
 - Only if combining interpolated images w. different information of the same object – e.g. different angles of moving object e.g. car
 - Super resolution (another topic)

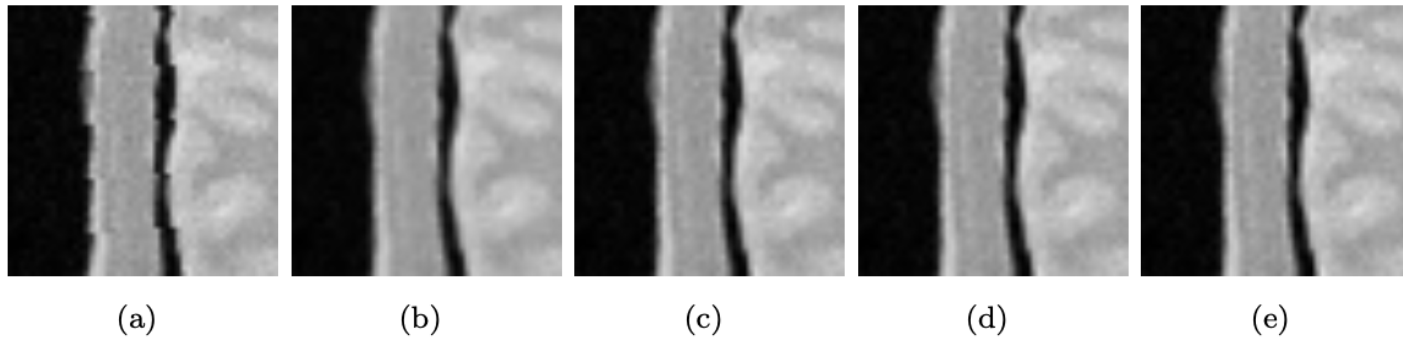
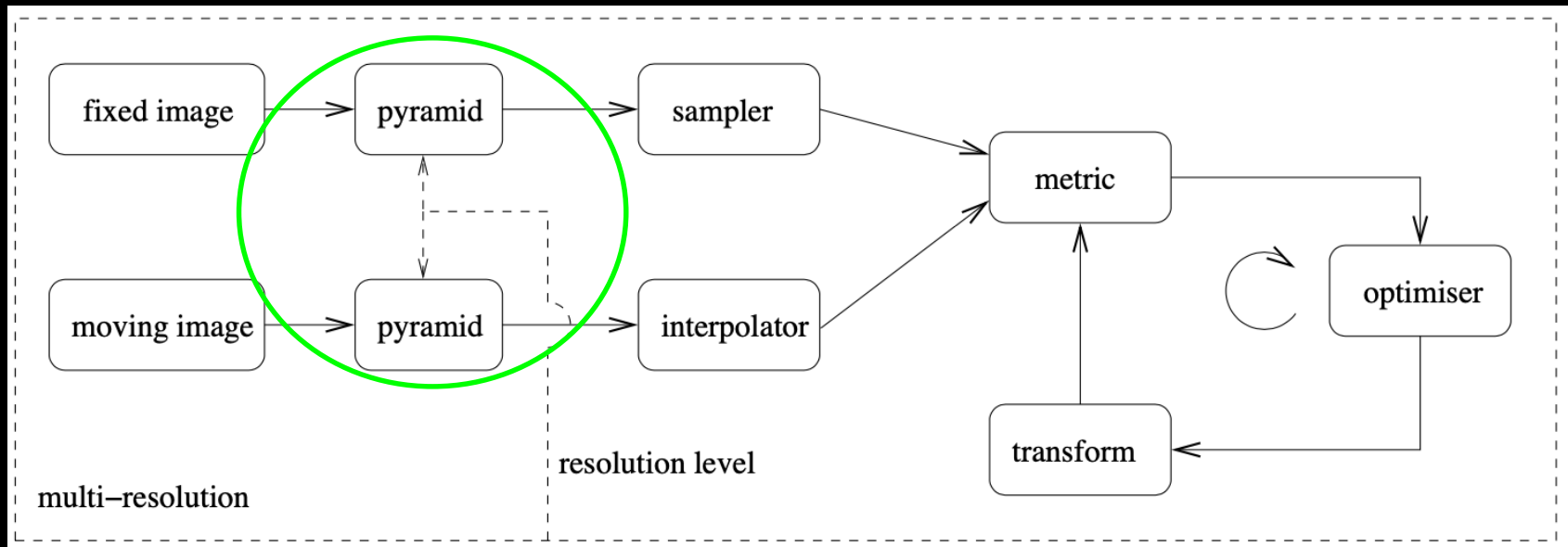


Figure 2.4: Interpolation. (a) nearest neighbour, (b) linear, (c) B-spline $N = 2$, (d) B-spline $N = 3$, (e) B-spline $N = 5$.

Image Registration pipeline

■ Pyramid



The Pyramid Principle

- To ensure robust image registration

Some stones?

Pretty close

Walking distance

From a bird

From space?



Very detailed

Good overview

Too coarse

The Pyramid Principle

- To ensure robust image registration

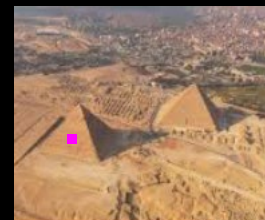
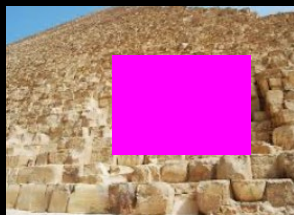
Some stones?

Pretty close

Walking distance

From a bird

From space?



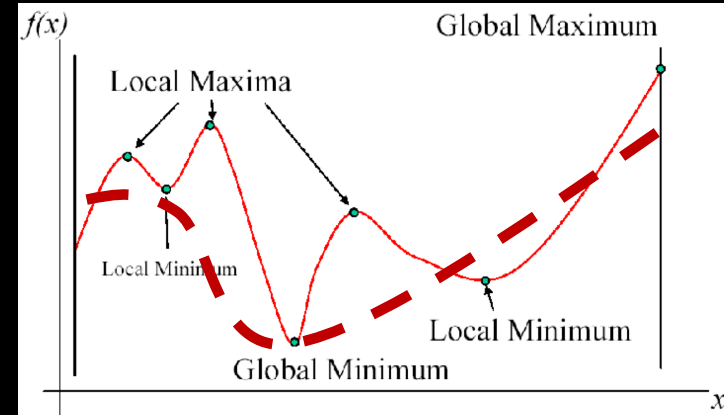
Very detailed

Good overview

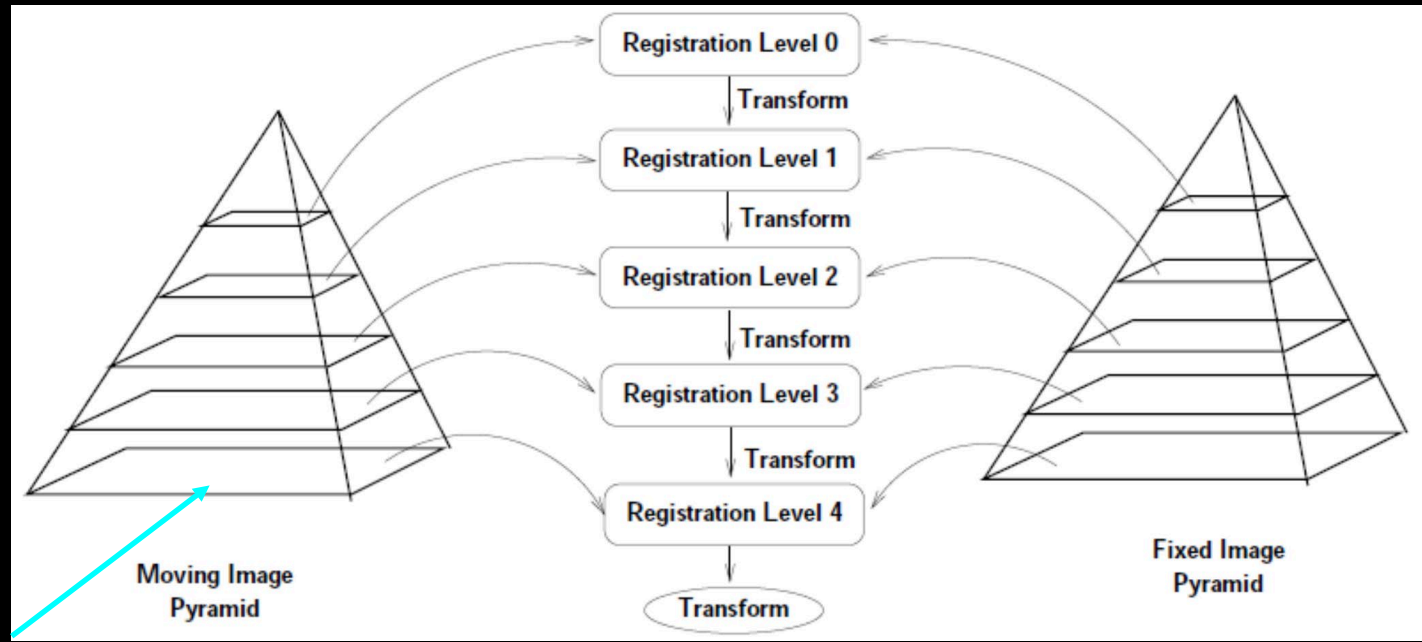
Too coarse

The Pyramid Principle

- A Multi-resolution strategy
- To ensure robust image registration
 - To reduce local minima's
 - What is a proper image resolution level ?



Coarser structural details



Original resolution



The Pyramid Principle

- Lower image resolution
 - Down sampling (memory reduction, fewer data)
- Less structural details
 - Smoothing (Complex method settings become more general)

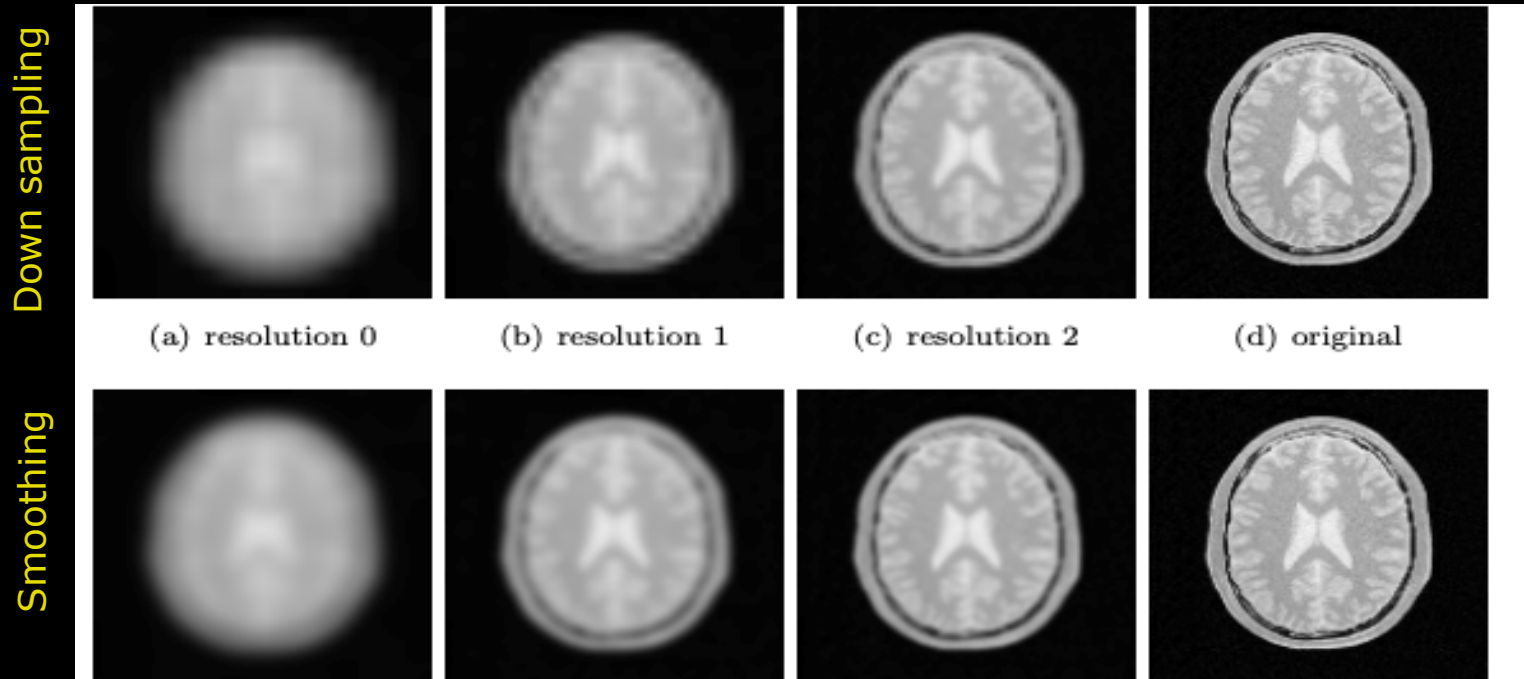
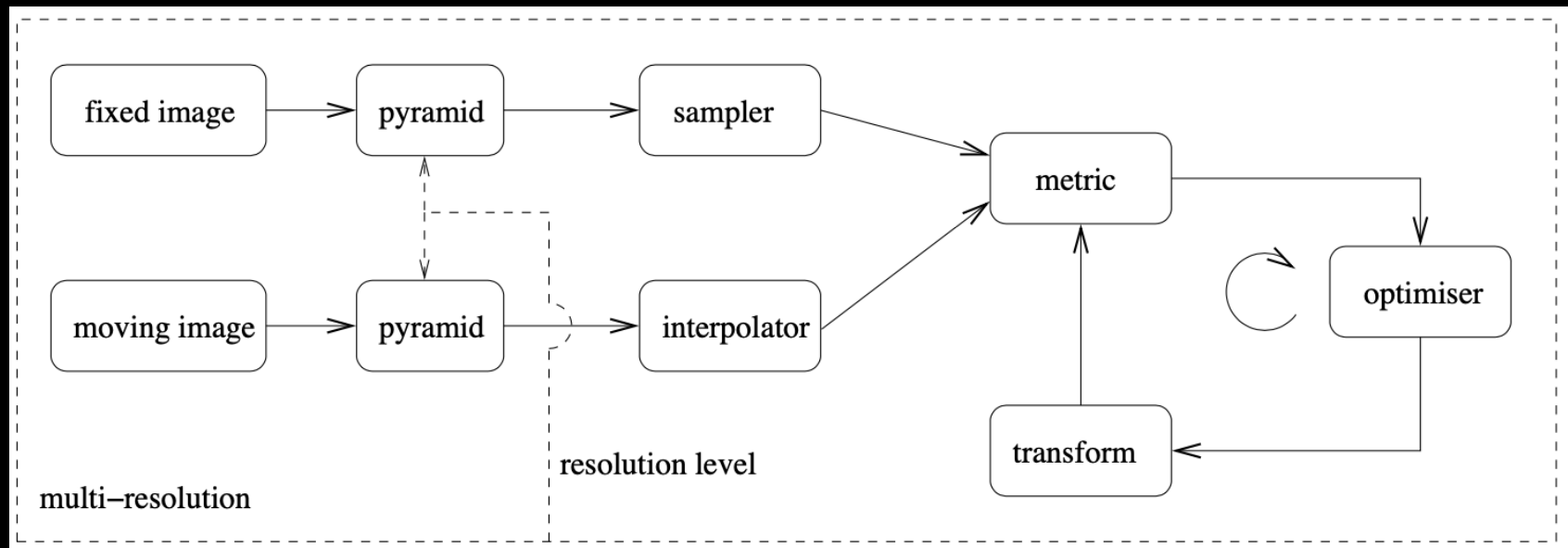


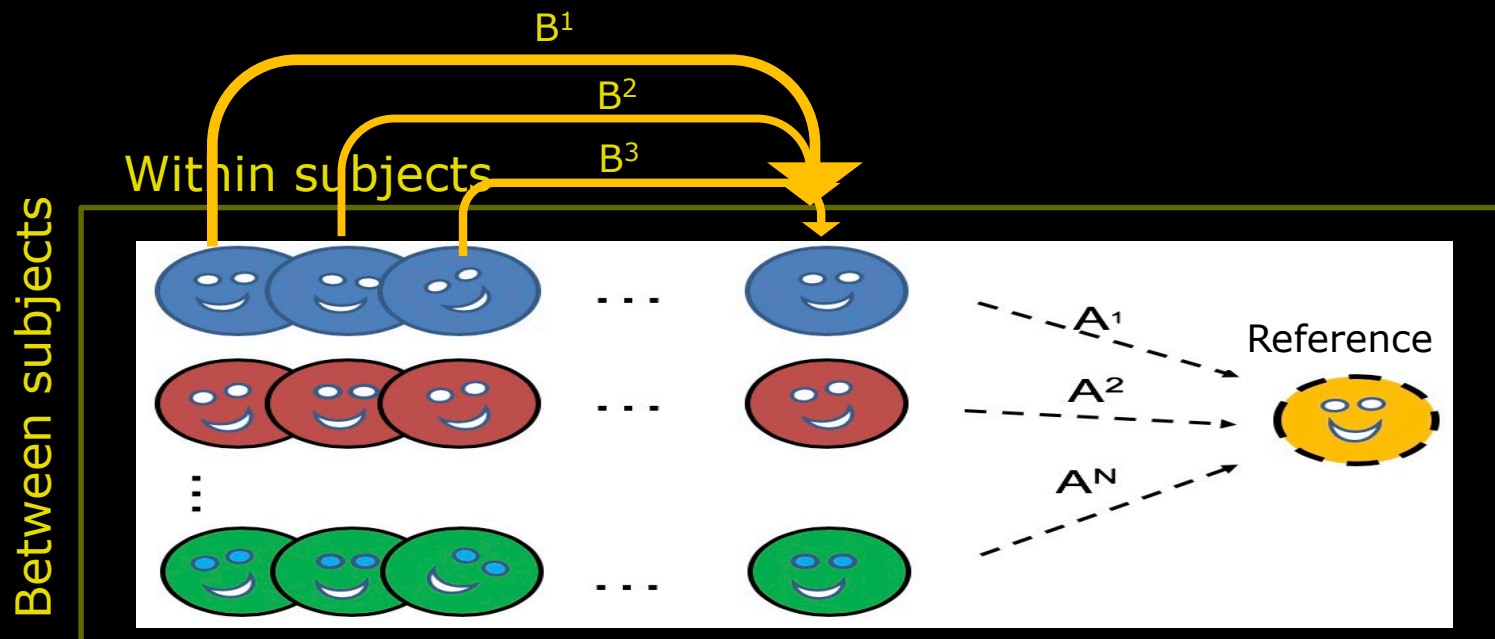
Image Registration pipeline

- At the end we just select an existing tool
- Still, we need how too select method settings 😊
 - This was the first step in the registration pipeline



Combining Image Registration pipelines

- First step : Within subjects (Same structure + temporal)
- Second step: Between subjects (different structure+ temporal)
 - Can use an iterative procedure to improve registration
- Combine subject-wise transformation metrics by multiplication
 - Apply only one interpolation at the end to minimise blurring





Quiz 6: Quality inspection - How

How to quality assurance (QA) the image registration results?

- A) Use a similarity measure
- B) Visual inspection
- C) No need it to - just works
- D) Sum of square difference
- E) Search the internet for experience

Image Registration pipeline strategy

- Within subjects and between challenges
 - E.g. Histology 2D \rightarrow 3D: Structural difference between slices
 - Visually inspect your results!!

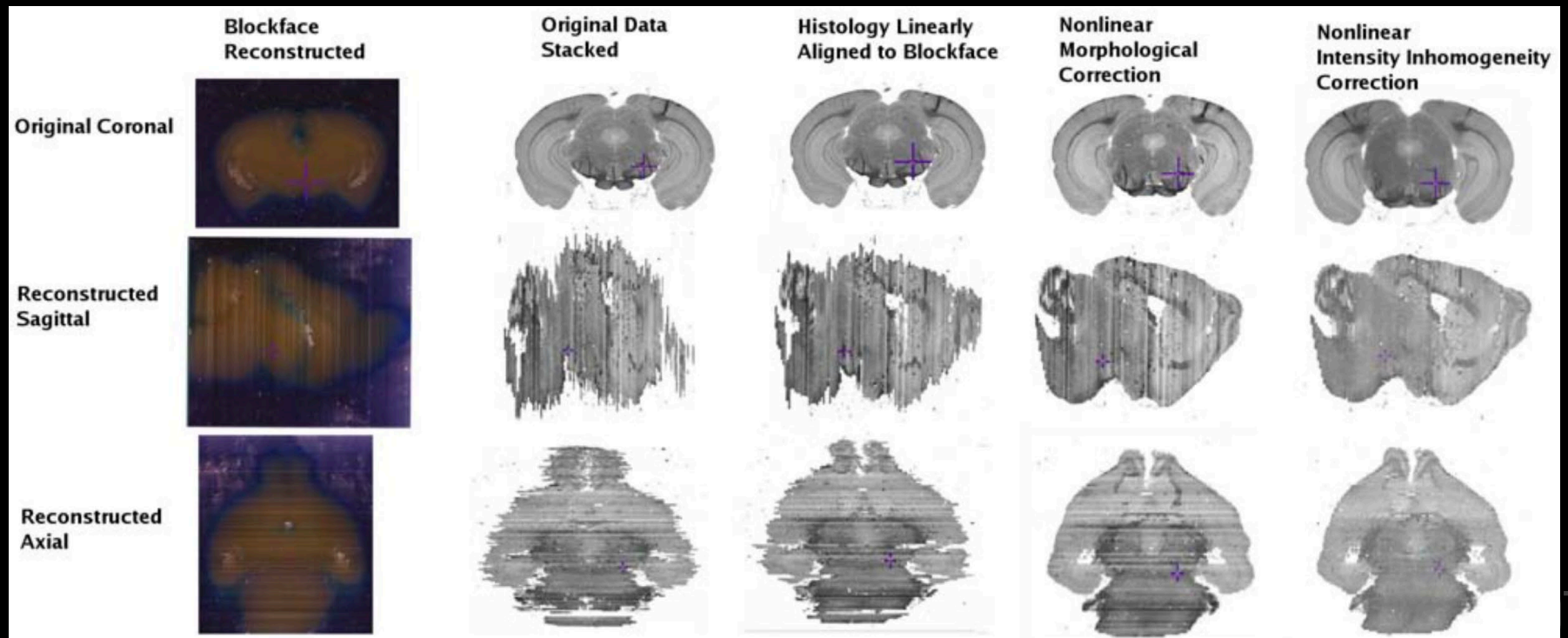
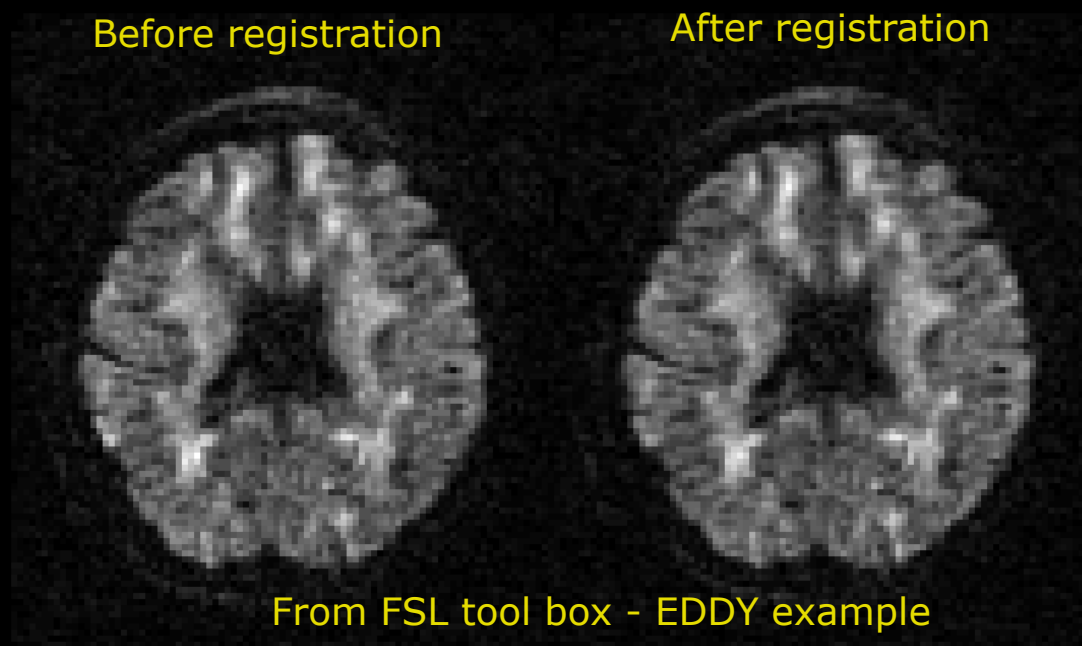


Image Registration pipeline strategy

- Within subjects across time points (temporal)
 - Remove image distortions + subject motion
- Visually inspect your results!!





What did you learn today?

- Describe difference between a pixel and voxel
- Choose a general image-to-image registration pipeline
- Apply 3D geometrical affine transformations
- Use the Homogeneous coordinate system to combine transformations
- Compute a suitable similarity metric given the image modalities to register
- Compute the normalized correlation coefficient (NNC) between two images
- Compute Entropy
- Describe the concept of iterative optimizers
- Compute steps in the gradient descent optimization steps
- Apply the pyramidal principle for multi-resolution strategies
- Select a relevant registration strategy: 2D to 3D, Within- and between objects and moving images

Next week – Real-time face detection using Viola Jones method

